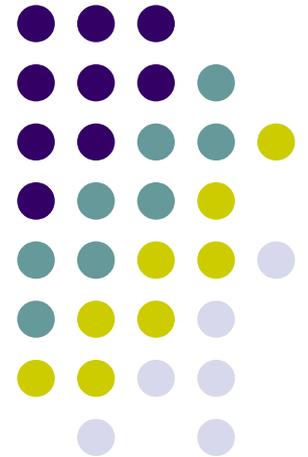


# Controles de Calidad de IMRT.

**Dr. Eduardo Francisco Larrinaga Cortina**



---

**Créditos:**

**Dr. Rodolfo Alfonso Laguardia**

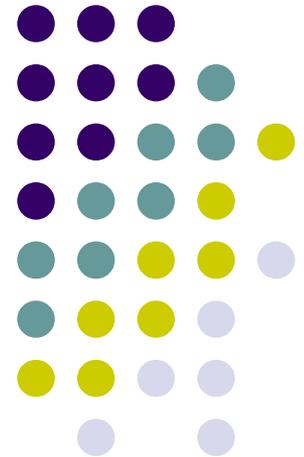
**Curso Nacional Introducción IMRT.**

**HHA Cuba 2008**

**Maestría en Física Médica**

**Dosimetría Clínica en Radioterapia**

**Curso 2011-2012**





Créditos

[https://www.youtube.com/watch?v=cSKhST4B\\_cI](https://www.youtube.com/watch?v=cSKhST4B_cI)

# **Intensity Modulated Radiation Therapy: Dosimetric Aspects & Commissioning Strategies**

**ICTP School on Medical Physics for Radiation Therapy**

**Justus Adamson PhD**

**Assistant Professor**

**Department of Radiation Oncology**

**Duke University Medical Center**



INCORPORATION OF IMAGING STEADILY IMPROVING RT ACCURACY

IMAGING

DOSE

- X-ray or CT scan for treatment planning

External Beam Radiation Therapy  
(2-D RT)

- Broad target zone

- CT scan for treatment planning

3-D Conformal Radiation Therapy  
(3-D CRT)

- Homogenous radiation delivery
- More conformal

- CT scan for treatment planning

Intensity-Modulated  
Radiation Therapy (IMRT)

- Heterogeneous radiation delivery
- More conformal than 3-D CRT

- Fusion of CT, PET, MRI
- Scans for treatment planning, positioning, dose measurement

Image-Guided  
Radiation Therapy

- Heterogeneous radiation delivery
- Dose can be modified between fractions

- Images taken for treatment planning, positioning, intradose determination, fusion of images

Real-Time  
IGRT

- Heterogeneous radiation delivery
- Delivery dose can change within fraction

□ Current □ Emerging ■ Future

Source: Elekta; Innovators Center Interviews and analysis.

# IMRT QA – Quo Vadis ?

J. Battista

R. Barnett

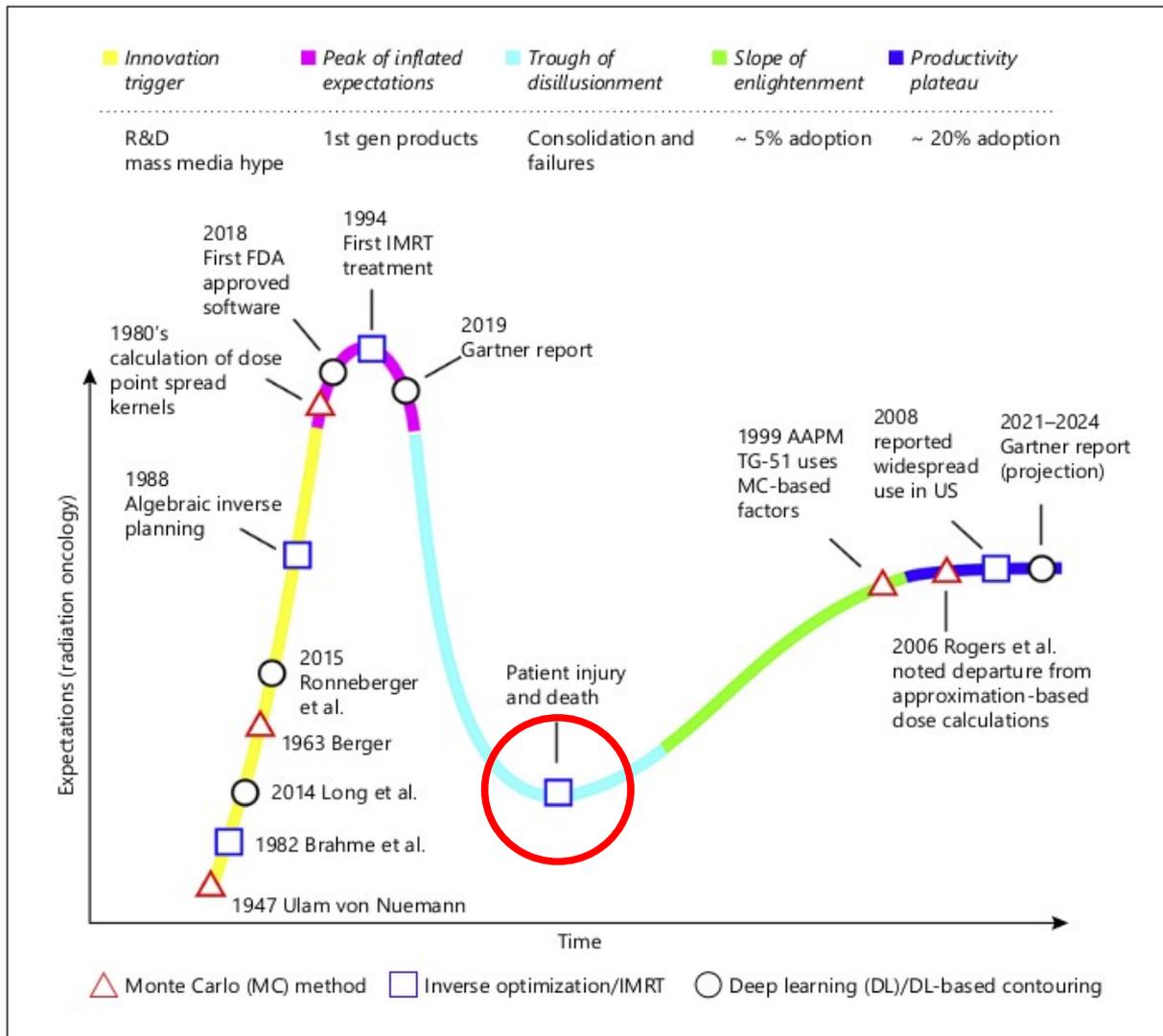
December 14, 2011



# Contenidos

- **Controles de calidad a la unidad de tratamiento**
- **Controles de calidad paciente específicos de tratamientos de IMRT**
  - **Equipamiento disponible**
  - **Pruebas de principio a fin (end-to-end).**
  - **Inteligencia artificial**
  - **Evaluación de resultados**

# Principales Innovaciones en Radioterapia



The Emergence of Artificial Intelligence within Radiation Oncology Treatment Planning. Netherton T, Oncology 2021.



THE RADIATION BOOM

# Radiation Offers New Cures, and Ways to Do Harm

BY WALT BOGDANICH

JANUARY 24, 2010

As Scott Jerome-Parks lay dying, he clung to this wish: that his fatal radiation overdose — which left him deaf, struggling to see, unable to swallow, burned, with his teeth falling out, with **ulcers** in his mouth and throat, nauseated, in severe pain and finally unable to breathe — be studied and talked about publicly so that others might not have to live his nightmare.



1 of 4

Scott Jerome-Parks, with his wife, Carmen, was 43 when he died in 2007 from a radiation overdose.

# New York Incident



## A Plan Goes Wrong

On a brisk day in March 2005, Mr. Jerome-Parks prepared for his fifth radiation session at St. Vincent's. The first four had been delivered as prescribed. Now Dr. Berson wanted the plan reworked to give more protection to Mr. Jerome-Parks' teeth.

...physicist was trying to save her work, the computer began seizing up, displaying an error message. The hospital would later say that similar system crashes "are not uncommon with the Varian software..."

So at 6:29 p.m., she ran a test to verify that the treatment plan was carried out as prescribed. What she saw was horrifying: **the multi-leaf collimator, which was supposed to focus the beam precisely on his tumor, was wide open.**





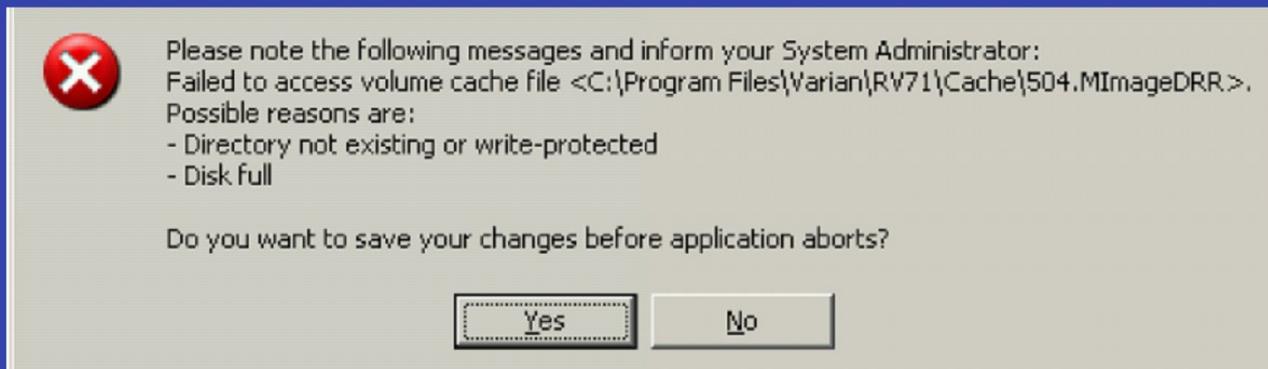


- **March 11:** Physician wants **modified dose distribution** (reducing dose to teeth) “1AOropharyn” is copied and saved to the DB as “1BOropharyn”
- **March 14:** Re-optimization for “1B Oropharyn”.
  - New optimal fluences saved to DB.
  - MLC motion control points for IMRT generated. Normal completion.

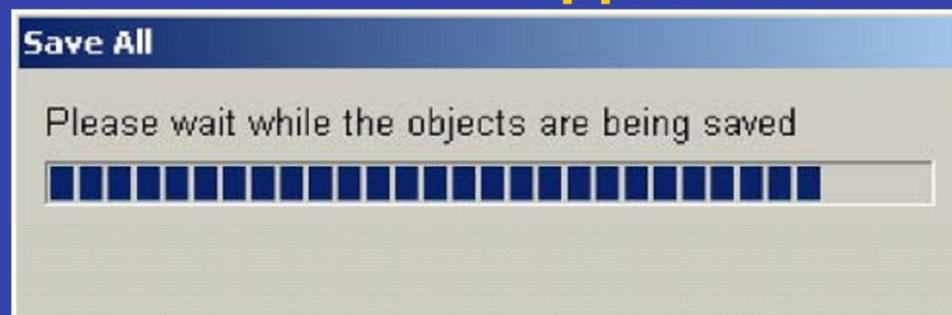
## • **March 14**

- “Save all” is started. All new and modified data should be saved to the DB.
- In this process, data is sent to a **holding area** on the server, and **not saved permanently until ALL data elements have been received.**
- Data to be saved included: (1) fluence data, (2) DRRs and (3) MLC control points

- **March 14, 11 a.m.**
  - An error message is displayed.
  - The user presses “Yes”, which begins a second, separate, save transaction.
  - MLC control point data is moved to the holding area.



- The software would have **appeared to be frozen.**



- **March 14, 11 a.m.**

- **No verification plan**, no pre-treatment dosimetry, no review by 2<sup>nd</sup> physicist
- Several computer crashes ignored and over-ridden.
- Plan approved by physician

## What they didn't notice:

The screenshot shows a radiotherapy planning software interface. The main window displays a table of field parameters for a treatment plan named '1B Oropharynx'. The table has columns for Field Order/Type, S/Treat, 6/Treat, 7/Treat, 8/Treat, and 9/Treat. The rows include Field ID, Field Name, Technique, Energy/Mode, Dose Rate (MU/min), MU, Time (min), Tol. Table, SSD (cm), Gantry/Source Fltn (Deg), Coll Fltn (Deg), Field X (cm), K1 (cm), X2 (cm), Field Y (cm), Y1 (cm), Y2 (cm), MLC, and Dynamic Wedge. A red circle highlights the 'Y1' and 'Y2' rows, which show values of 7.0 and 7.3 for Y1, and 8.0 and 8.5 for Y2. Another red circle highlights a yellow box in the 3D anatomical model on the right, which is labeled 'LPO-DRR1 - 3/14/2005 11:37 AM'.

Field Order/Type	5 / Treat	6 / Treat	7 / Treat	8 / Treat	9 / Treat
Field ID	3B PA Sinus	1B LPO	2B LAO Sinus	4B RAO Sinus	5B RPO Sinus
Field Name	AP Sinus	LPO	LPO Sinus	RAO Sinus	RPO Sinus
Technique	STATIC	STATIC	STATIC	STATIC	STATIC
Energy / Mode	6X	6X	6X	6X	6X
Dose Rate (MU / min)	300	300	300	300	300
MU	309	291	334	258	282
Time (min)	1.44	1.31	1.56	1.21	1.32
Tol. Table	IMRT_HN	IMRT_HN	IMRT_HN	IMRT_HN	IMRT_HN
SSD (cm)	91.2	90.7	94.2	94.4	90.7
Gantry/Source Fltn (Deg)	190.0	150.0	60.0	300.0	210.0
Coll Fltn (Deg)	90.0	90.0	90.0	90.0	90.0
Field X (cm)	11.0	11.3	11.3	11.3	10.9
K1 (cm)	+1.5	+1.5	+1.5	+1.5	+1.4
X2 (cm)	+9.5	+9.5	+9.5	+9.5	+9.5
Field Y (cm)	14.3	15.0	15.0	15.0	15.0
Y1 (cm)	+7.0	8.0	8.0	8.0	+8.0
Y2 (cm)	+7.3	+6.5	+6.0	+8.5	+8.5
MLC	NONE	NONE	NONE	NONE	NONE
Dynamic Wedge					
Int Mount					

# Impact of accident

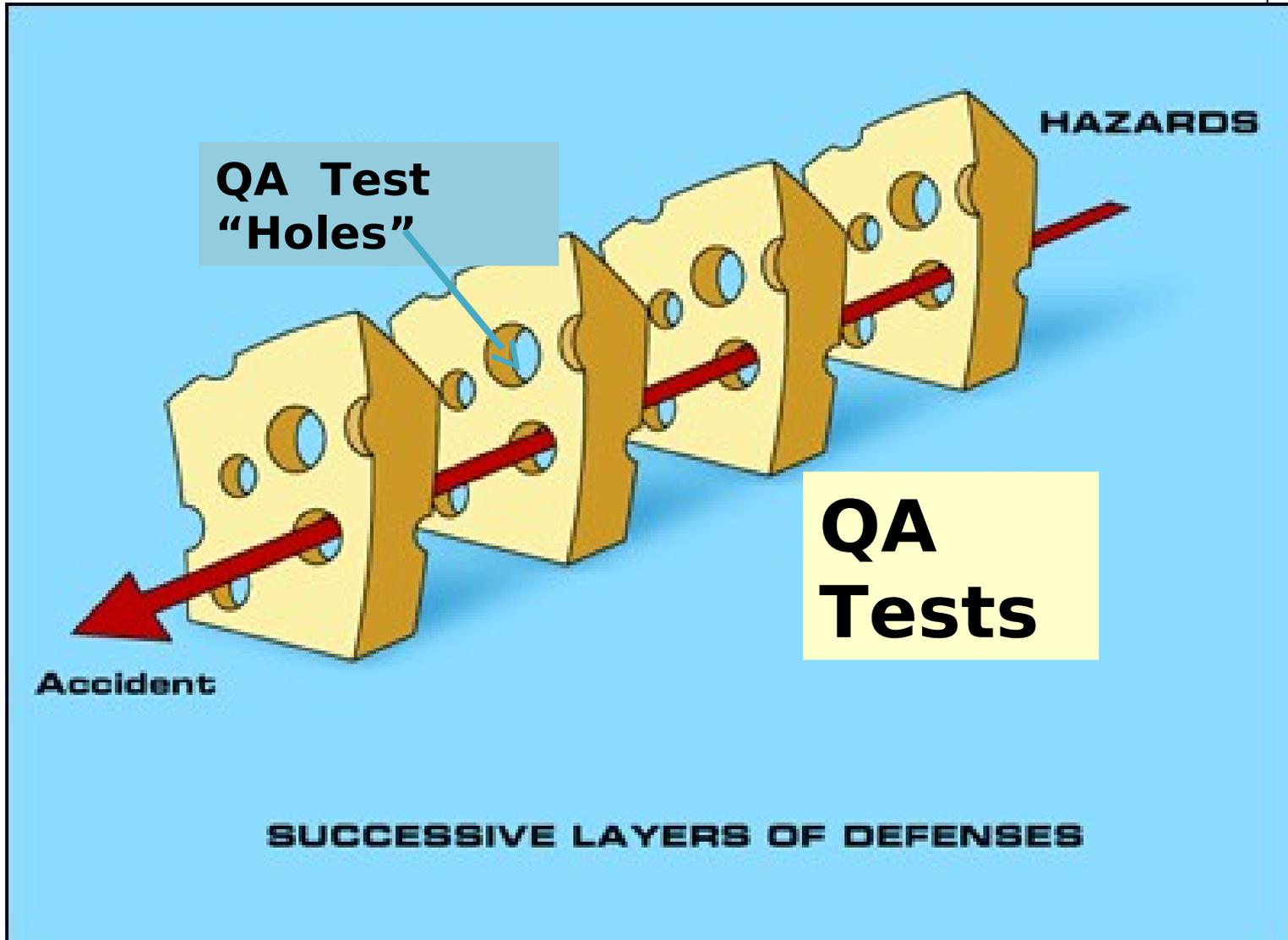
- The patient received 13 Gy per fraction for three fractions, i.e. **39 Gy in 3 fractions**

## Was there a bug in the Varian software:

**Of course, but the software had a lot of help:**

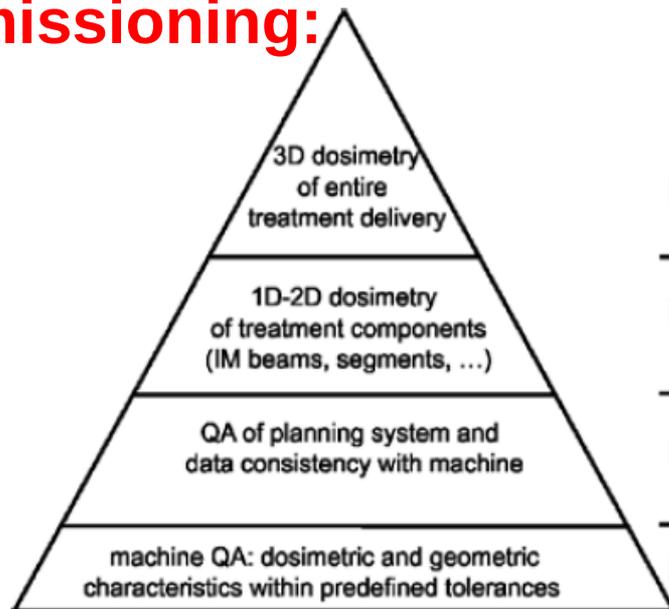
- 1. Error messages ignored and not investigated**
- 2. Treatment plan QA not performed**
- 3. No 2<sup>nd</sup> physics check**
- 4. MD rushed the plan modification**
- 5. Therapists weren't watching MLC display**

# Accident Prevention



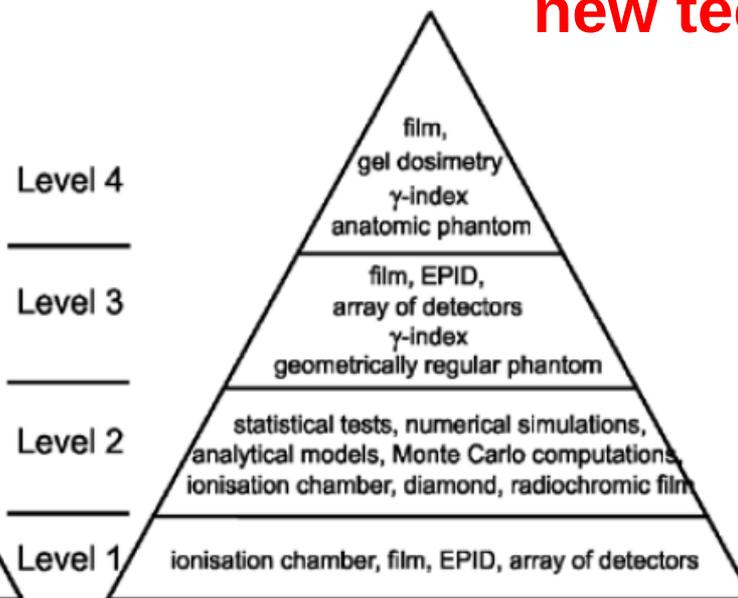
## Suggested Layers of Quality Assurance:

initial  
commissioning:



(a)

introducing a  
new technique:



(b)

**Figure 3.1** (a) Conceptual pyramid that correlates the various levels of dosimetric QA in IMRT. Like the situation for a real pyramid, each level is based on the stability of the underlying levels. The two lower levels can be part of the periodic QA procedures of equipment used for IMRT planning and delivery. For QA of a new clinical IMRT solution, one may start at the top by applying a 3D dosimetric verification of an entire treatment. One descends the pyramid to the lower levels if the 3D dosimetric verification reveals unacceptable discrepancies with treatment planning. (b) Methodology and tools appropriate for each of the levels. (Courtesy Carlos De Wagter, Ghent University Hospital, Ghent, Belgium, and the Institute of Physics).

# Puesta en servicio clínico IMRT



- **Unidad de tratamiento**
  - Pruebas mecánicas
  - Pruebas dosimétricas
  - Pruebas específicas de IMRT
- **Sistema de Planeación de Tratamiento (TPS)**
  - Pruebas 3DCRT
  - Pruebas IMRT
- **Verificación dosimétrica por plan.**
- **Verificación independiente redundante/Acreditación**
- **Control de calidad paciente-específico.**

# Control de Calidad IMRT

Unidad de Tratamiento



- **Pruebas 3DCRT**
- **Pruebas IMRT**
  - **Dosimétricas**
  - **Desempeño del MLC**



# Puesta en servicio clínico IMRT

## Unidad de tratamiento, Tolerancias



TABLE II. Monthly.

Procedure	Machine-type tolerance		
	Non-IMRT	IMRT	SRS/SBRT
<b>Dosimetry</b>			
X-ray output constancy			
Electron output constancy		2%	
Backup monitor chamber constancy			
Typical dose rate <sup>a</sup> output constancy	NA	2% (@ IMRT dose rate)	2% (@ stereo dose rate, MU)
Photon beam profile constancy		1%	
Electron beam profile constancy		1%	
Electron beam energy constancy		2%/2 mm	
<b>Mechanical</b>			
Light/radiation field coincidence <sup>b</sup>		2 mm or 1% on a side	
Light/radiation field coincidence <sup>b</sup> (asymmetric)		1 mm or 1% on a side	
Distance check device for lasers compared with front pointer		1 mm	
Gantry/collimator angle indicators (@ cardinal angles) (digital only)		1.0°	
Accessory trays (i.e., port film graticule tray)		2 mm	
Jaw position indicators (symmetric) <sup>c</sup>		2 mm	
Jaw position indicators (asymmetric) <sup>d</sup>		1 mm	
Cross-hair centering (walkout)		1 mm	
Treatment couch position indicators <sup>e</sup>	2 mm/1°	2 mm/1°	1 mm/0.5°
Wedge placement accuracy		2 mm	
Compensator placement accuracy <sup>f</sup>		1 mm	
Latching of wedges, blocking tray <sup>g</sup>		Functional	
Localizing lasers	±2 mm	±1 mm	< ±1 mm
<b>Safety</b>			
Laser guard-interlock test		Functional	
<b>Respiratory gating</b>			
Beam output constancy		2%	
Phase, amplitude beam control		Functional	
In-room respiratory monitoring system		Functional	
Gating interlock		Functional	



# AAPM Task Group 198 Report: An implementation guide for TG 142 quality assurance of medical accelerators

**Joseph Hanley<sup>1</sup> | Sean Dresser<sup>2</sup> | William Simon<sup>3</sup> | Ryan Flynn<sup>4</sup> |  
Eric E. Klein<sup>5</sup> | Daniel Letourneau<sup>6</sup> | Chihray Liu<sup>7</sup> | Fang-Fang Yin<sup>8</sup> |  
Bijan Arjomandy<sup>9</sup> | Lijun Ma<sup>10</sup> | Francisco Aguirre<sup>11</sup> | Jimmy Jones<sup>12</sup> |  
John Bayouth<sup>13</sup> | Todd Holmes<sup>14</sup>**

<sup>1</sup>Princeton Radiation Oncology, Monroe, New Jersey 08831, USA

<sup>2</sup>Winship Cancer Institute, Radiation Oncology, Emory University, Atlanta, Georgia 30322, USA

<sup>3</sup>Sun Nuclear Corp, Melbourne, Florida 32940, USA

<sup>4</sup>Department of Radiation Oncology, University of Iowa, Iowa City, Iowa, 52242,

## Abstract

The charges on this task group (TG) were as follows: (a) provide specific procedural guidelines for performing the tests recommended in TG 142; (b) provide estimate of the range of time, appropriate personnel, and qualifications necessary to complete the tests in TG 142; and (c) provide sample daily, weekly, monthly, or annual quality assurance (QA) forms. Many of the guidelines in this report are



- 2.E.2.3. Annual checks
- 2.E.3. Siemens virtual wedge
  - 2.E.3.1. Daily checks
  - 2.E.3.2. Monthly checks
  - 2.E.3.3. Annual checks
- 2.F. Multileaf collimators (MLCs)
  - 2.F.1. Weekly
    - 2.F.1.1. Qualitative test (Picket Fence)
  - 2.F.2. Monthly
    - 2.F.2.1. Leaf position accuracy (non-IMRT)
    - 2.F.2.2. Backup diaphragm settings
    - 2.F.2.3. Leaf travel speed
    - 2.F.2.4. Leaf position accuracy (IMRT)
  - 2.F.3. Annual
    - 2.F.3.1. MLC transmission
    - 2.F.3.2. Leaf position repeatability
    - 2.F.3.3. MLC spoke shot
    - 2.F.3.4. Coincidence of light-radiation fields
    - 2.F.3.5. Moving window IMRT
- 2.G. Radiographic imaging
  - 2.G.1. Daily—kV and MV (EPID) imaging

- 2.G.7.1. Beam quality or energy
  - 2.G.7.2. Imaging dose
  - 2.G.8. Annual—CBCT (kV and MV)
    - 2.G.8.1. Imaging dose
3. SUMMARY OF RECOMMENDATIONS OR IMPLEMENTATION SCHEME
- 

## 1 | INTRODUCTION

### 1.A | Purpose

The American Association of Physicists in Medicine (AAPM) Task Group (TG) 142 report,<sup>1</sup> “Quality Assurance of Medical Accelerators,” published in 2009, updated table II of TG 40<sup>2</sup> with respect to frequency and tolerances of existing procedures. It also added recommendations for quality assurance (QA) of ancillary devices [asymmetric jaws, multileaf collimators (MLCs), dynamic or virtual wedges] that were not covered in TG 40. The recommendations made in TG 142 were dependent on the types of procedures performed on the linear accelerator (linac). Separate tests and tolerances were recommended based on whether spe-

# Control de Calidad IMRT

## Unidad de Tratamiento. Desempeño MLC



- Suite de pruebas suministradas por el fabricante
  - Ejemplo Varian: DMLC QA Test Patterns

Product Documentation x +

myvarian.com/s/productdocumentation?lang=es

### Biblioteca de documentación

Inicio > Biblioteca de documentación

La biblioteca de documentación de Varian contiene manuales, CTBs, notificaciones y otros materiales de referencia relacionados con el producto. [Contáctenos](#) si necesita ayuda para encontrar un documento específico.

Mis Favoritos

Grupo de Productos: --Any--  
Tipo de Documento: --Any--  
Versión: --Any--  
Búsqueda por palabra clave: dmlc

APLICAR  
REINICIAR

Título	Fecha	Traducción	Tipo de Documento	Versión
★ <a href="#">DMLC QA Test Patterns and Procedures (rev H)</a>	Jul 1, 2014		Downloads	6.8, 7.1, 7.2, 7.3, 7.5, 8.0, 8.1
★ <a href="#">DMLC QA Test Patterns and Procedures Guide</a>	Jul 1, 2014		Reference Materials	6.8, 7.1, 7.2, 7.3, 7.5, 8.0, 8.1

# Control de Calidad IMRT

## Unidad de Tratamiento. Desempeño MLC



- Suite de pruebas suministradas por el fabricante
  - Ejemplo Varian: DMLC QA Test Patterns

Drive

Buscar en Drive

Ordenadores > ... > DMLC QA Test Pattern... > Mill120

Tipo Personas Modificado (Enviar comentarios a Google)

Nombre	Propietario	Última modifi...	Tamaño de a
ReadMe.txt	yo	28 feb 2014	164 bytes
TEST1A.DVA	yo	17 jul 2008	15 kB
TEST1B.DVA	yo	17 jul 2008	10 kB
TEST1C.DVA	yo	17 jul 2008	15 kB
TEST2A.DVA	yo	17 jul 2008	10 kB
TEST2B.DVA	yo	17 jul 2008	10 kB
TEST2C.DVA	yo	27 ago 2008	5 kB
TEST2D.DVA	yo	17 jul 2008	5 kB
TEST3A.DVA	yo	17 jul 2008	75 kB
TEST3B.DVA	yo	17 jul 2008	75 kB
TEST3C.DVA	yo	17 jul 2008	75 kB

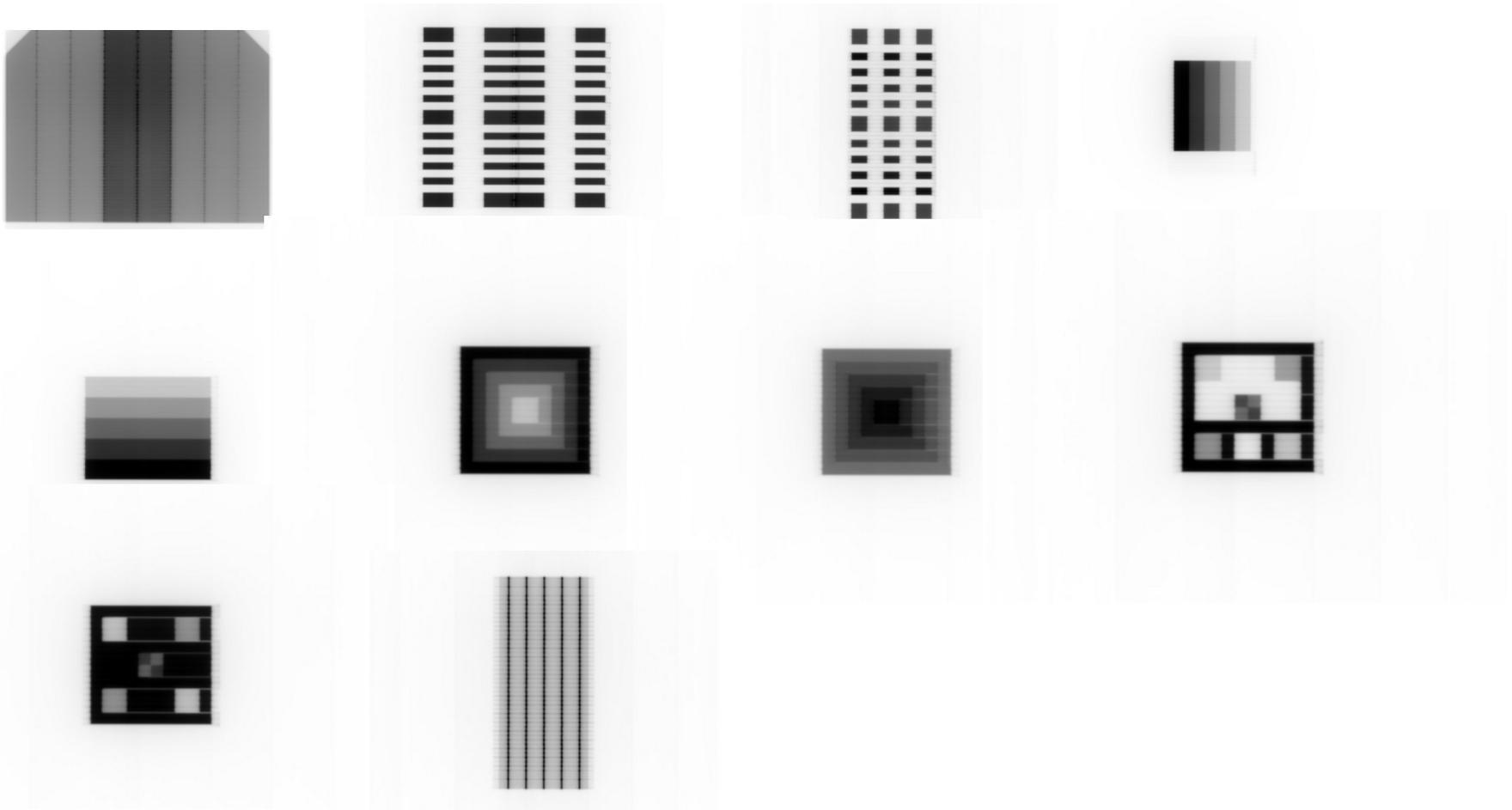
16,46 GB de 30 GB usado

Gestionar almacenamiento

# Control de Calidad IMRT

## Unidad de Tratamiento. Desempeño MLC

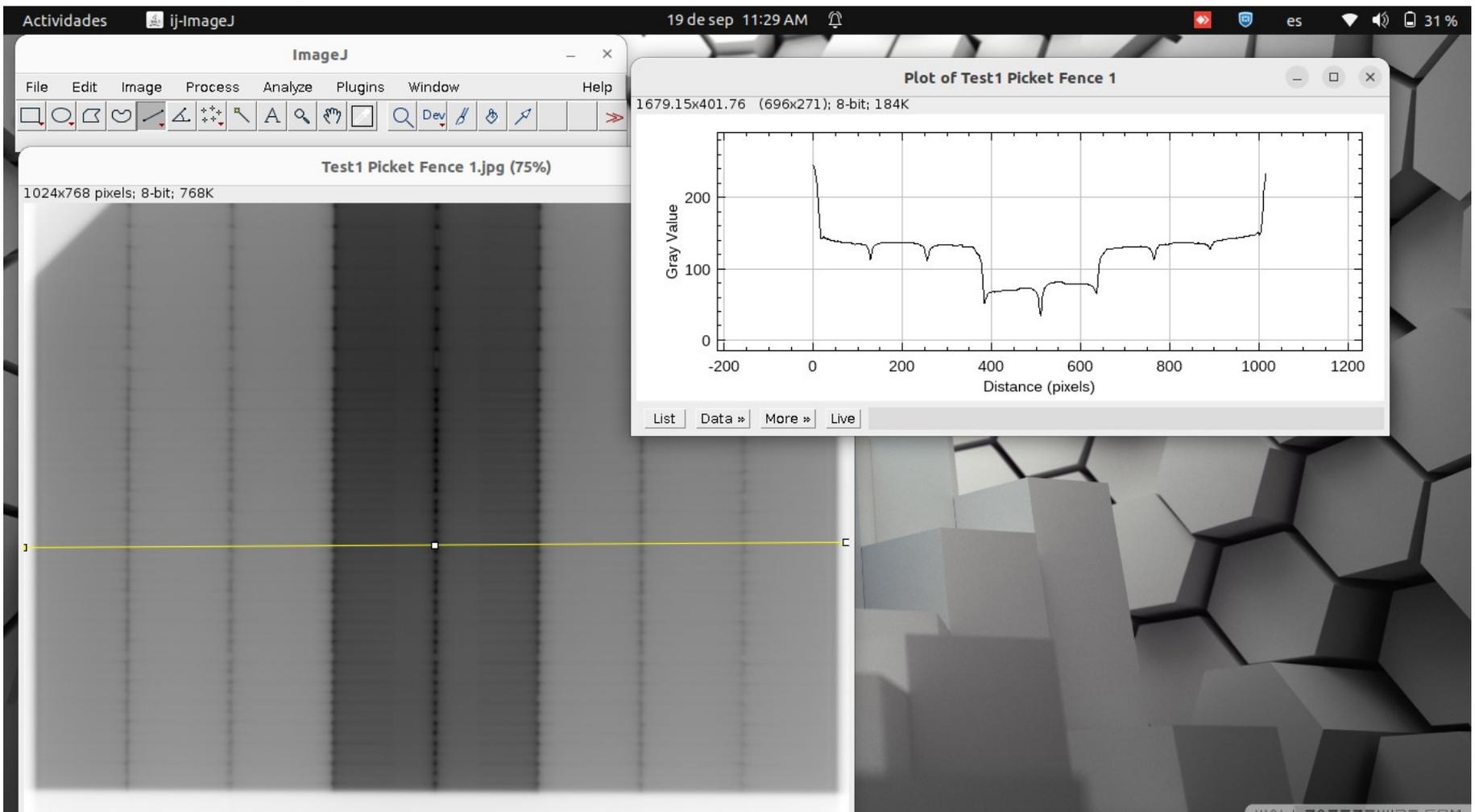
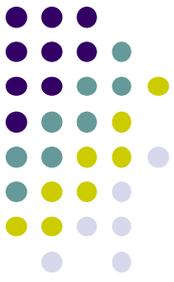
- Suite de pruebas suministradas por el fabricante
  - Ejemplo Varian: DMLC QA Test Patterns



# Control de Calidad IMRT

## Unidad de Tratamiento. Desempeño MLC

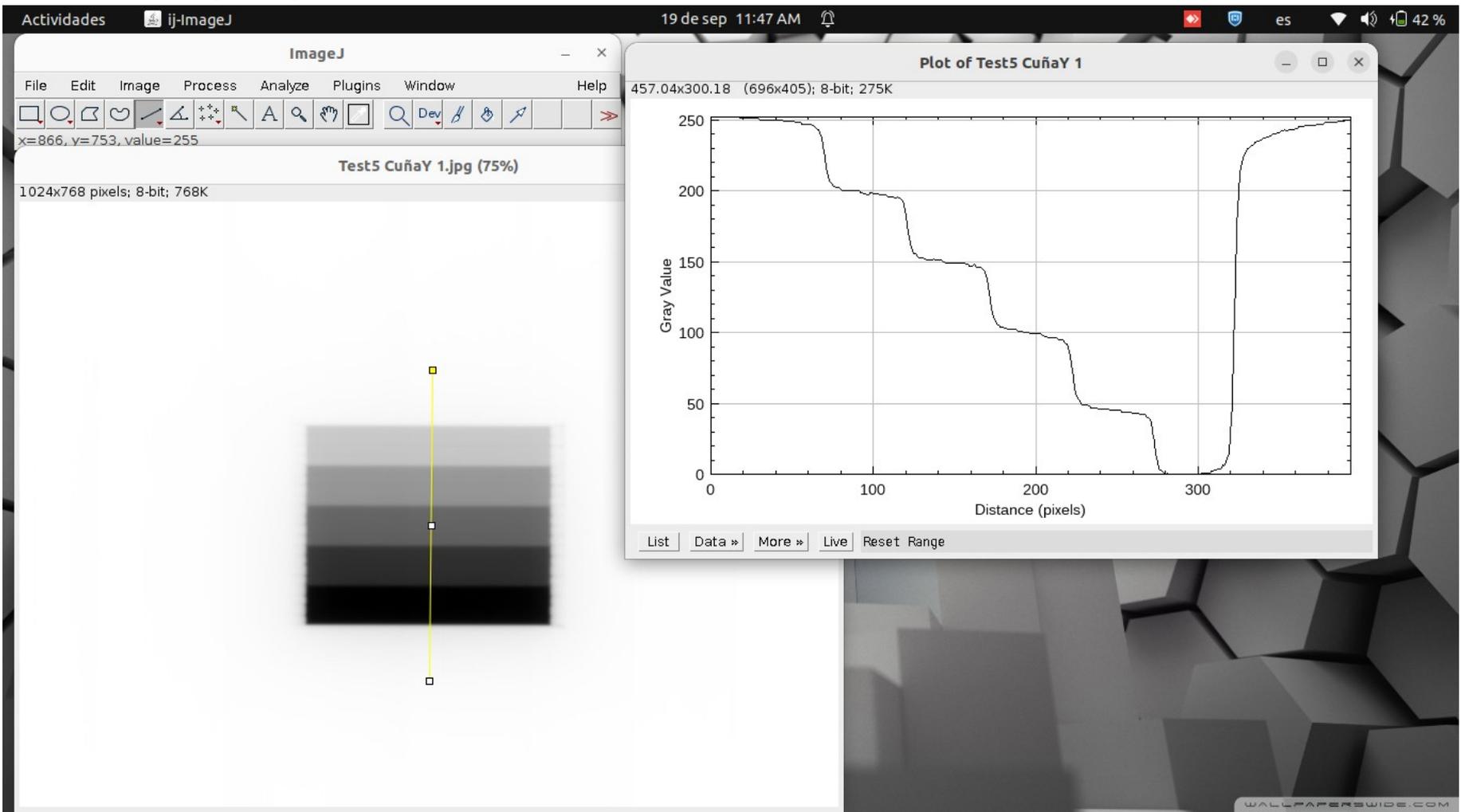
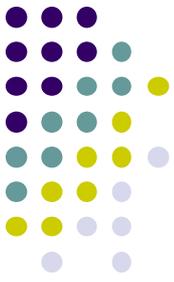
- Suite de pruebas suministradas por el fabricante
  - Ejemplo Varian: DMLC QA Test Patterns



# Control de Calidad IMRT

## Unidad de Tratamiento. Desempeño MLC

- Suite de pruebas suministradas por el fabricante
  - Ejemplo Varian: DMLC QA Test Patterns

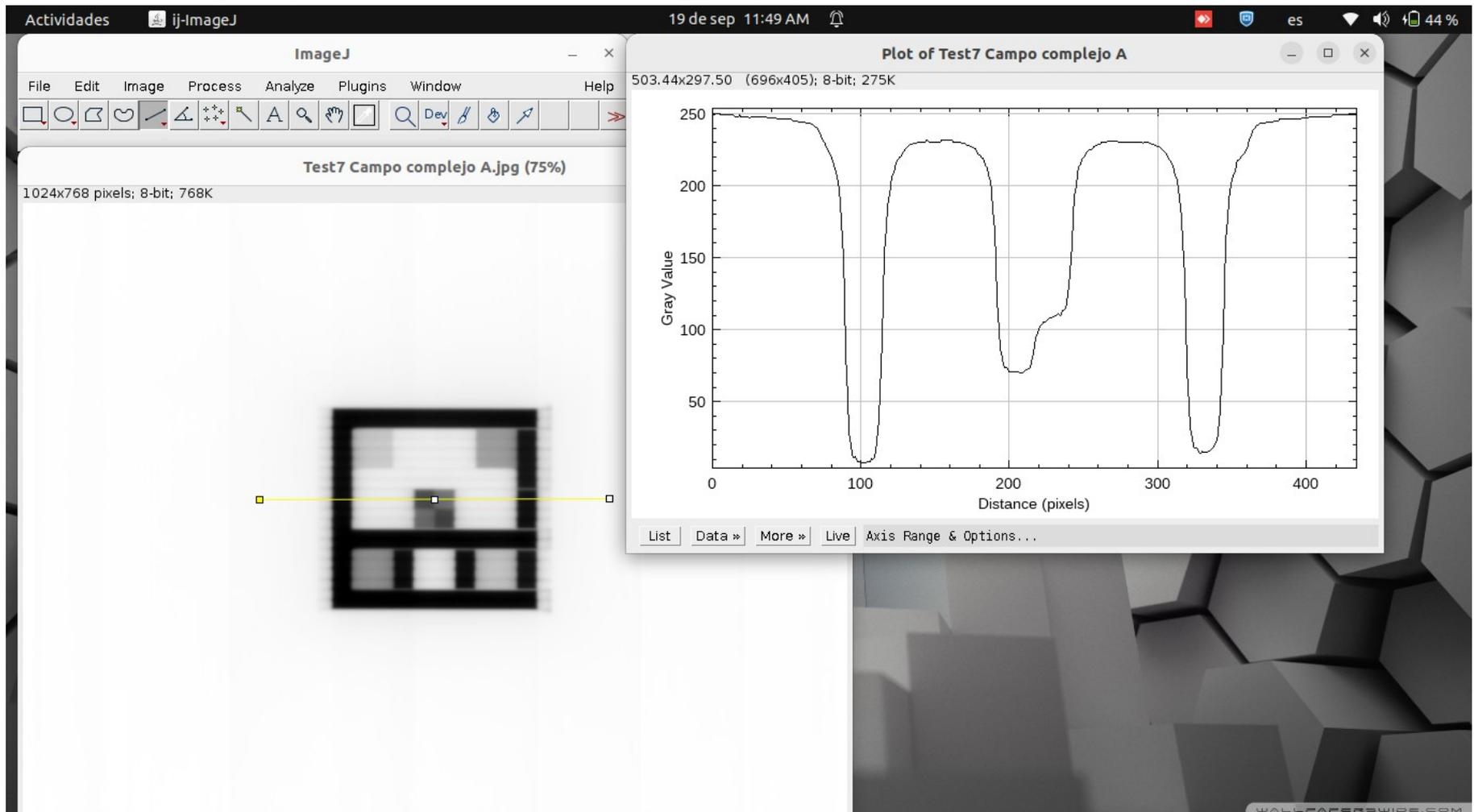




# Control de Calidad IMRT

## Unidad de Tratamiento. Desempeño MLC

- Suite de pruebas suministradas por el fabricante
  - Ejemplo Varian: DMLC QA Test Patterns



# Control de Calidad IMRT

## Unidad de Tratamiento. Desempeño MLC

- Suite de pruebas suministradas por el fabricante
  - Ejemplo ELEKTA: iComCAT/ ELEKTA MACHINE QA

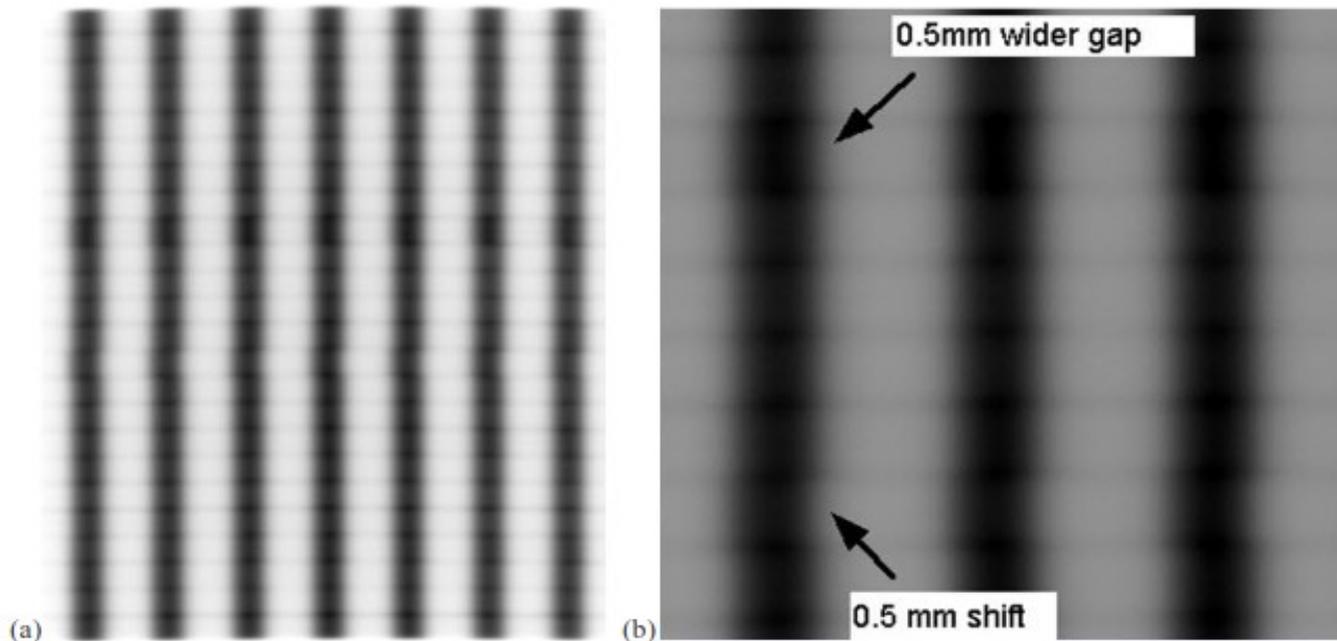


FIG. 7. Picket Fence with intentional errors of 0.5 mm wider gap and 0.5 mm horizontal shift shown for: a) 25 cm by 25 cm field, and b) magnified portion.

VMAT testing for an Elekta accelerator. Kurin D et al. JACMP, 2012

<https://www.elekta.com/focus/austrian-physicists-save-time-and-increase-efficiency-with-elekta-qa-solutions/>

# Control de Calidad IMRT

## Paciente-Específico



- **IMRT Planificaciones complejas**
  - **Difíciles de calcular los aportes de dosis manualmente**
  - **Pueden ser utilizados paquetes informáticos alternativos para el cálculo de los dosis (no tiene en cuenta la administración)**
  - **Pueden ser medidos las dosis (fluencias) impartidas por la unidad de tratamiento (prueba principio-fin)**
  - **Puede estimarse el desempeño y resultado de la administración del tratamiento del análisis de los ficheros de registro del MLC (log files)**
  - **Pueden estimarse los resultados del CC paciente-específico desde la planeación del tratamiento, Inteligencia Artificial**

# Control de Calidad IMRT

## Paciente-Específico. Programas independientes



← → ↻ <https://www.standardimaging.com/qa-software/imsure-qa-software> 📄 ☆ 📧 📱 📄 ☰

**STANDARD IMAGING** 

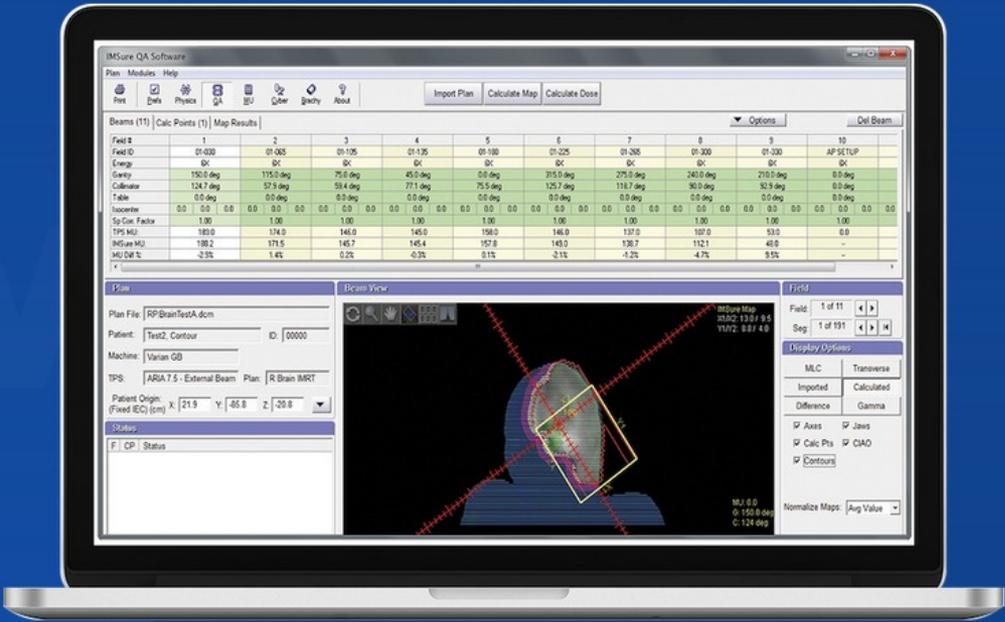
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Field #	1	2	3	4	5	6	7	8	9	10
Field ID	01-000	01-005	01-105	01-125	01-150	01-205	01-265	01-300	01-320	AP-54 TUP
Energy	6C	6C	6C	6C	6C	6C	6C	6C	6C	6C
Energy	150.0 deg	115.0 deg	75.0 deg	45.0 deg	0.0 deg	315.0 deg	275.0 deg	240.0 deg	210.0 deg	0.0 deg
Collimator	124.7 deg	57.9 deg	59.4 deg	77.1 deg	75.5 deg	125.7 deg	119.7 deg	90.3 deg	93.9 deg	0.0 deg
Table	0.0 deg	0.0 deg	0.0 deg	0.0 deg	0.0 deg	0.0 deg	0.0 deg	0.0 deg	0.0 deg	0.0 deg
Inocenter	0.0	0.0	0.0	0.0	0.0	0.0	0.0	0.0	0.0	0.0
Sp. Con. Factor	1.00	1.00	1.00	1.00	1.00	1.00	1.00	1.00	1.00	1.00
TPS MU	180.0	174.0	145.0	145.0	190.0	148.0	137.0	109.0	53.0	0.0
IMSure MU	180.2	173.5	145.7	145.4	157.8	149.0	136.7	112.1	48.0	-
MU Del %	-0.3%	1.4%	0.2%	-0.3%	0.1%	-0.1%	-0.2%	-4.7%	9.5%	-

**Plan** | Modules | Help

Plan File: RP\BrainTestA.dcm  
Patient: Test2, Contour ID: 00000  
Machine: Varian GB  
TPS: ARIA 7.5 - External Beam Plan: R Brain IMRT  
Patient Origin (Fixed IC) (cm): x: 21.9 y: 45.8 z: 30.8

Field: 1 of 11  
Seg: 1 of 191

Display Options:  
 MLC  Transverse  
 Imported  Calculated  
 Difference  Gamma  
 Axes  Jaws  
 Calc Pls  CIAO  
 Contours  
Normalize Maps: Avg Value

MU: 0.0  
D: 150.0 deg  
C: 124 deg

**Intro** ↓ **3 Source Model** ↓ **Advanced Features** ↓

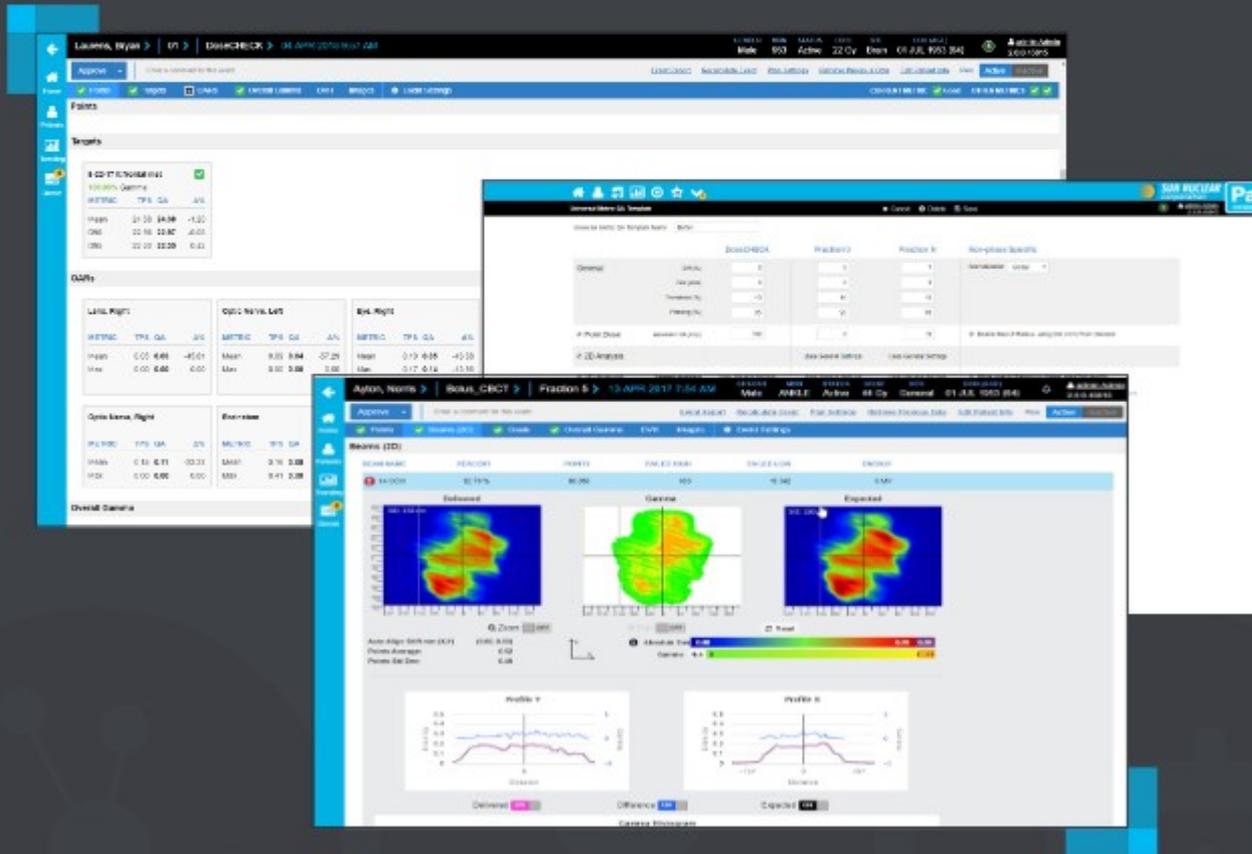
# Control de Calidad IMRT

Paciente-Específico. Programas independientes



## SunCHECK™ Patient

Comprehensive Patient QA



# Control de Calidad IMRT

## Paciente-Específico. Programas independientes



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## VERIQA Patient QA Platform



The Modular Software  
for Comprehensive Patient QA –  
Streamlining Workflows Based on Proven Technologies

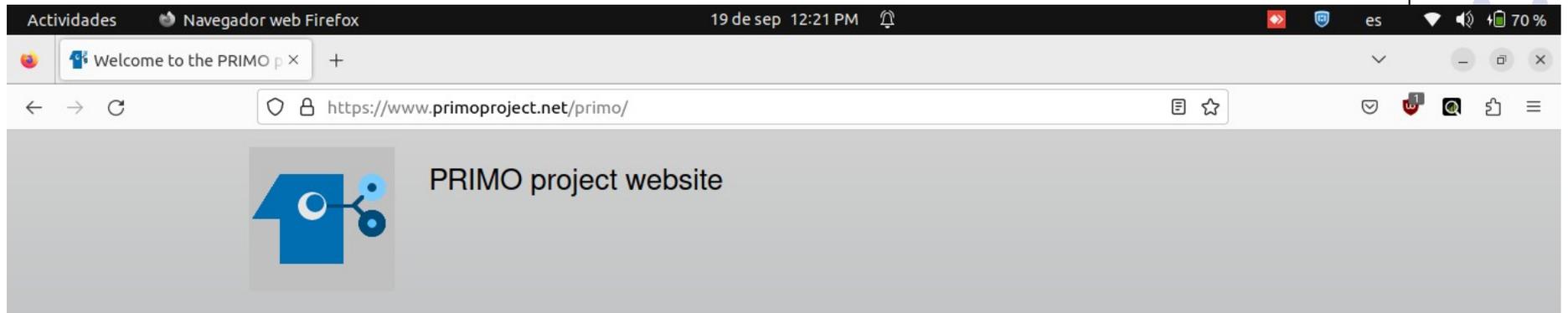
One Platform. Flexible and Scalable.

From Visualization and evaluation to verification and reporting. All in one modular platform, built on future-proof client-server architecture.



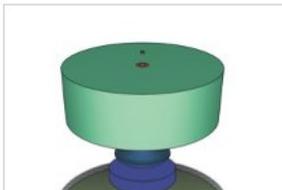
# Control de Calidad IMRT

## Paciente-Específico. Programas independientes



### Navigation

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## Welcome to the PRIMO project website.

PRIMO is a computer software that simulates clinical linear accelerators (linacs) and estimates absorbed dose distributions in phantoms and computerized tomographies. It combines a graphical user interface with the general-purpose radiation transport Monte Carlo code PENELOPE and the fast Monte Carlo code DPM (see [publications](#)).

These are its most relevant features:

- It simulates most Varian [1] and Elekta [2] linacs, with their electron applicators and multileaf collimators. Varian TrueBeam STx machines can also be simulated using the phase-space files distributed by the vendor, or alternatively, with an experimentally-based complete geometry called [FakeBeam](#). Elekta linacs are only supported in version 0.1.5.
- Absorbed dose distributions can be obtained in a phantom or in computerized tomographies provided in DICOM [3] format.
- Structures can be delineated (version 0.1.5) or, alternatively, they can be imported in DICOM-RT STRUCT [3] format.
- Treatment plans can be imported in DICOM-RT PLAN [3] format (version 0.3.1).
- Radiation fields can be stored in intermediate phase-space files that comply with the IAEA [4] format. Graphical and numerical analysis tools for phase-space files are provided.

# Control de Calidad IMRT

## Paciente-Específico. Pruebas end-to-end



- **Pruebas (principio-fin)**
  - **Mediciones en un punto**
    - C.I./diodo/otros detectores
  - **Mediciones en un plano**
    - películas radiográficas/radiocrómicas
    - arreglos de C.I./diodos
    - EPID
  - **Mediciones Compuestas**
  - **Mediciones volumétricas**
    - Gels
    - Fricke



# Control de Calidad IMRT

## Paciente-Específico. Pruebas end-to-end



- TC (True Composite), Compuesto
- PFF (Perpendicular Field by Field), Campo a campo perpendicular o colapsado
- PC (Perpendicular Composite), Compuesto perpendicular o colapsado

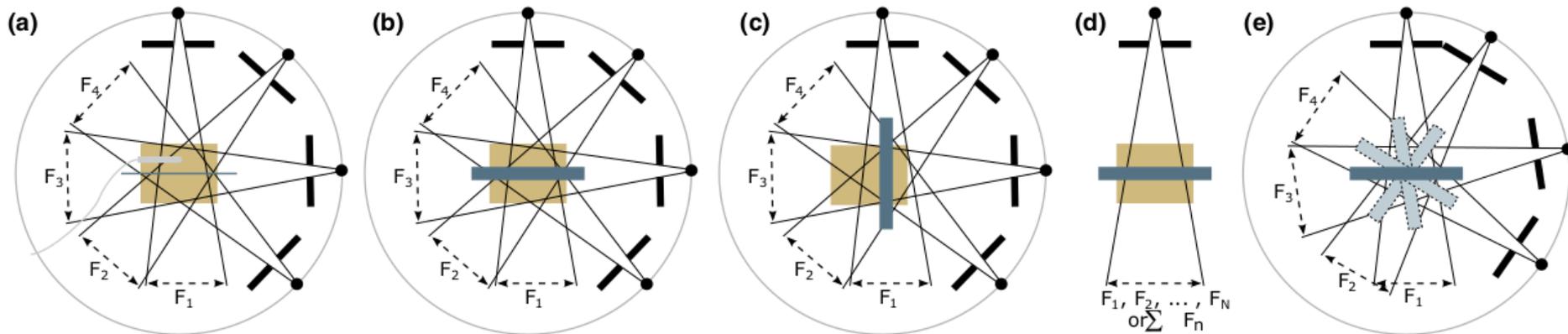


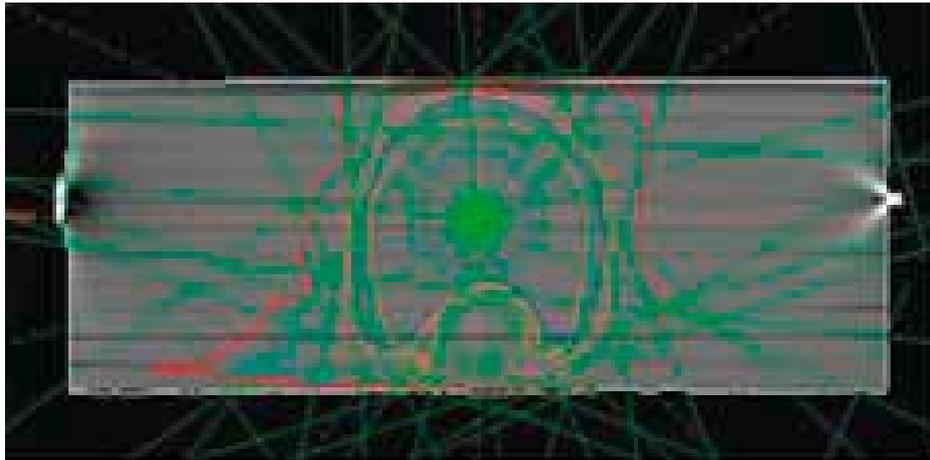
FIG. 6. (a) True composite (TC) delivery on a phantom with an IC placed at a specific depth and a radiographic film at a coronal orientation. (b) TC delivery on a stationary 2D array device placed in the coronal direction on the treatment table. (c) TC delivery on a stationary 2D array device placed in the sagittal direction on the treatment table. (d) Perpendicular field-by-field (PFF) or perpendicular composite (PC) delivery on a stationary 2D array device placed in the coronal direction on the treatment table. (e) PFF or PC delivery on 2D array device mounted on the treatment head.

# Control de Calidad IMRT

## Paciente-Específico. Pruebas end-to-end



- Mediciones en un punto

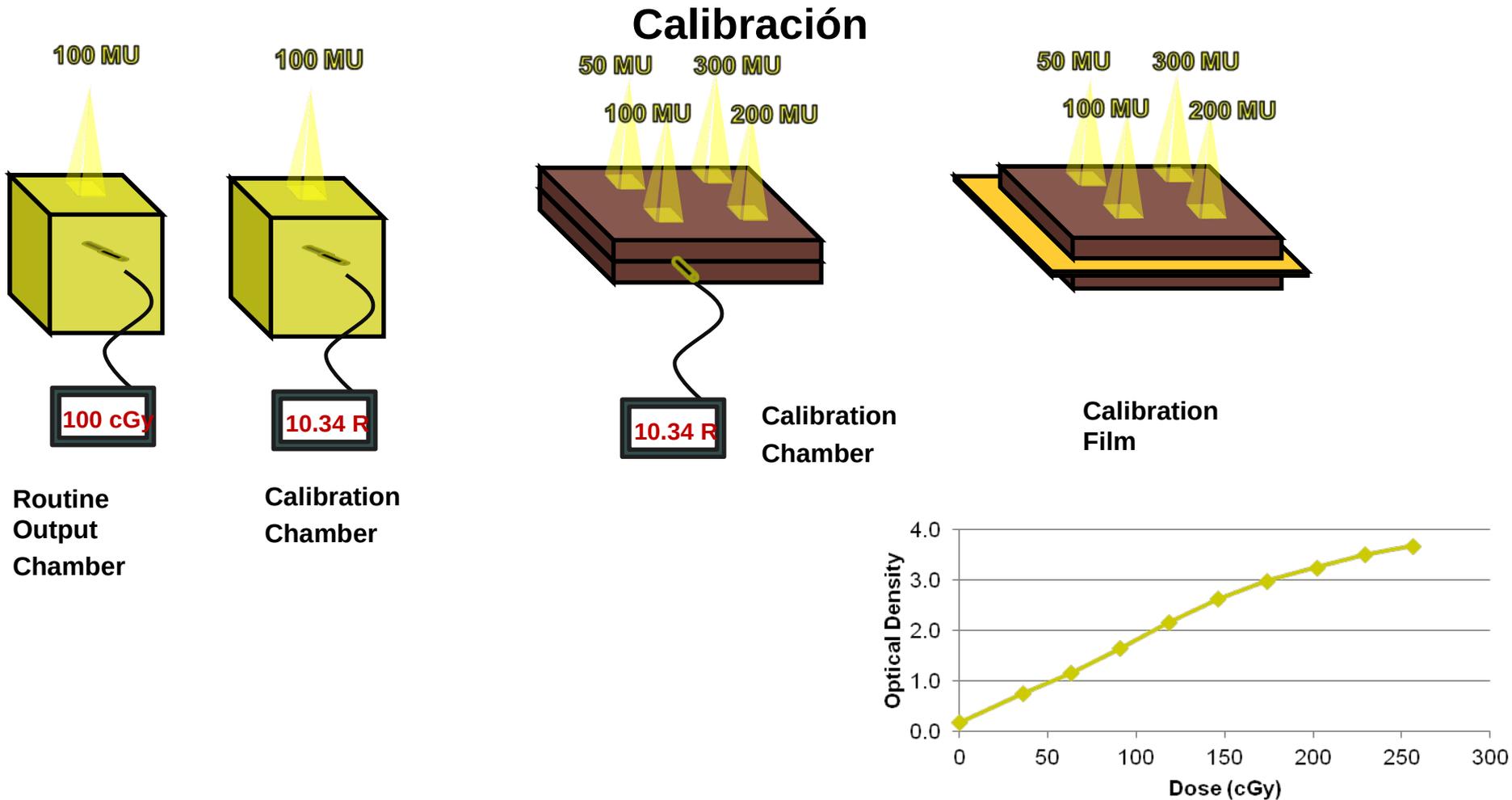


# Control de Calidad IMRT

## Paciente-Específico. Pruebas end-to-end



- Mediciones en un plano. Películas radiográficas

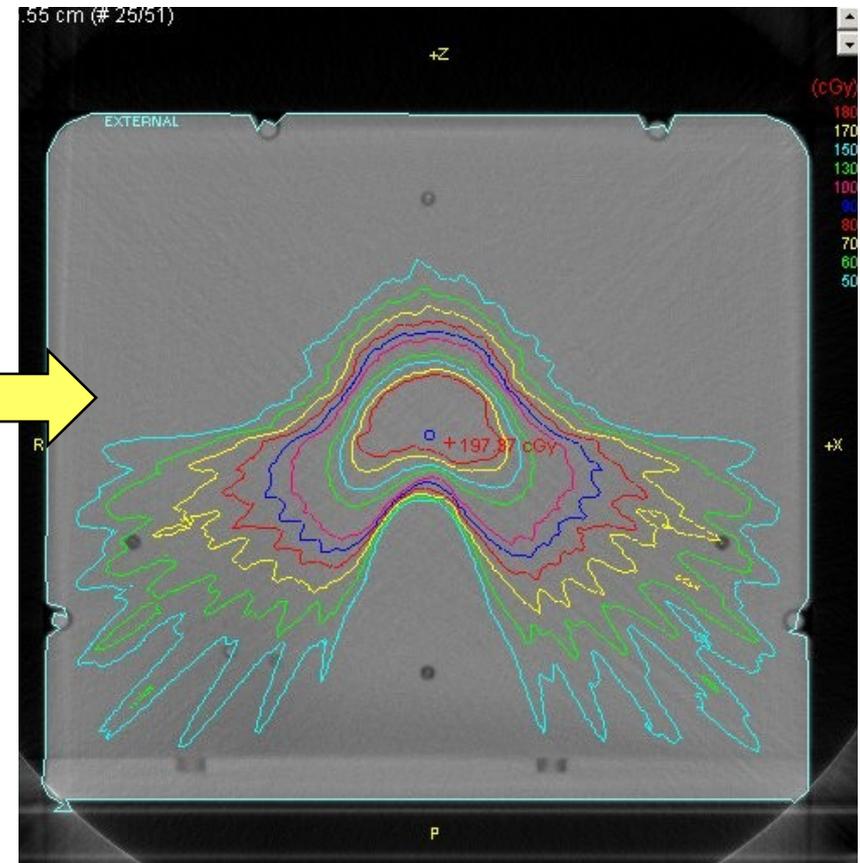
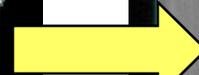
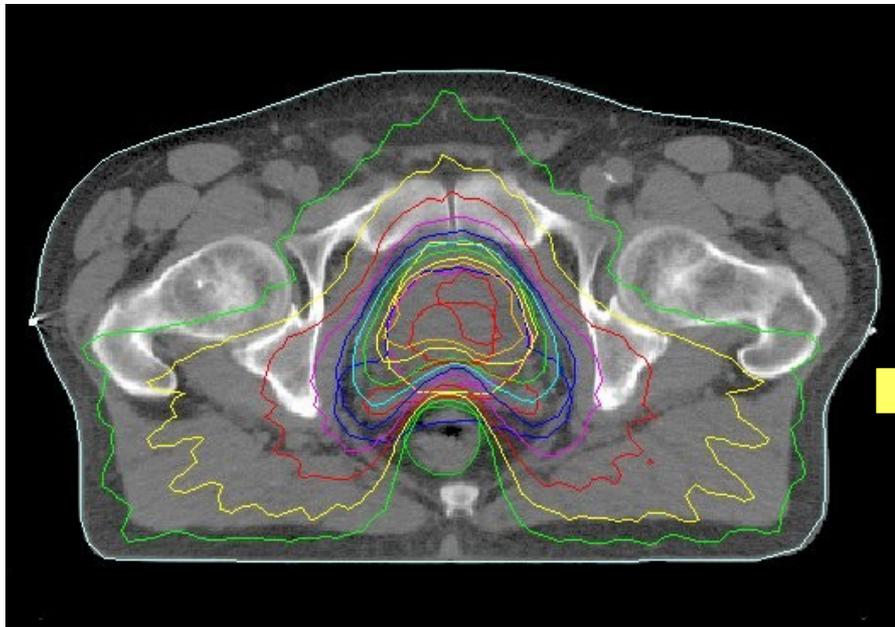


# Control de Calidad IMRT

Paciente-Específico. Pruebas end-to-end



- Mediciones en un plano. Películas radiográficas

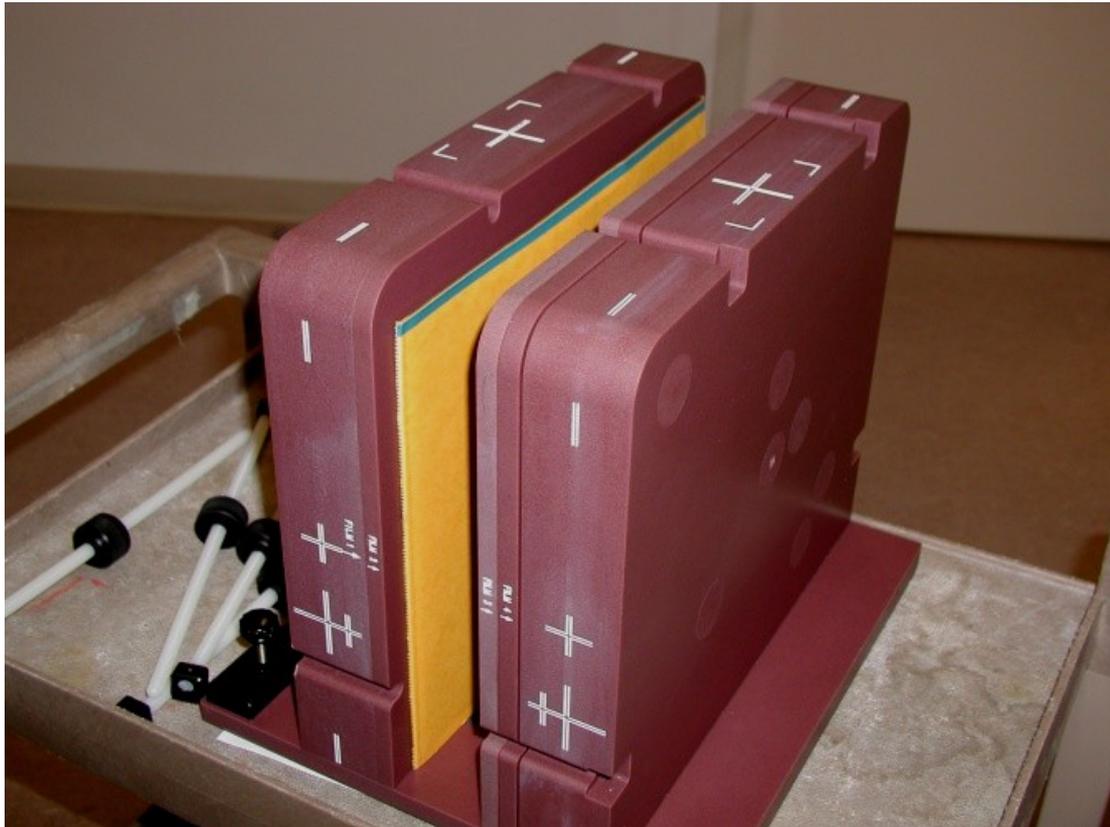


# Control de Calidad IMRT

## Paciente-Específico. Pruebas end-to-end



- **Mediciones en un plano. Películas radiográficas**  
Kodak Enhanced Dose Range (EDR) Film

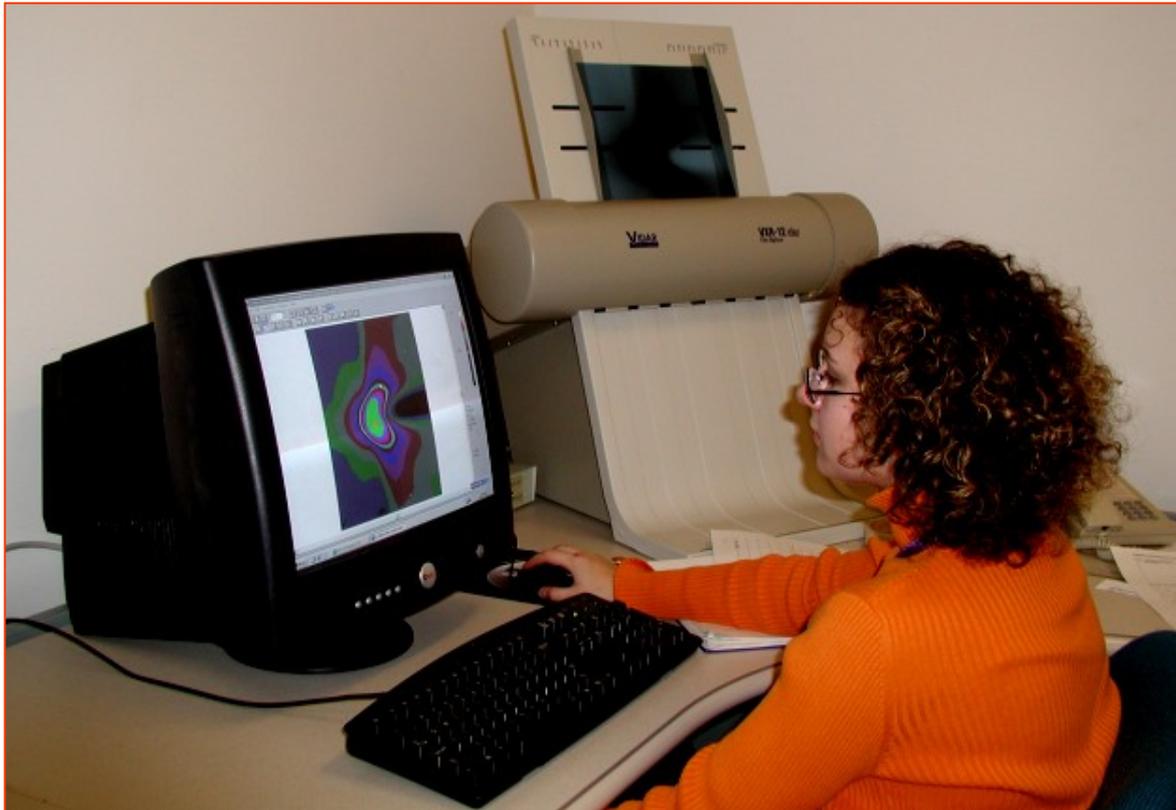


# Control de Calidad IMRT

## Paciente-Específico. Pruebas end-to-end



- **Mediciones en un plano. Películas radiográficas**  
**Procesamiento (Digitalización)**

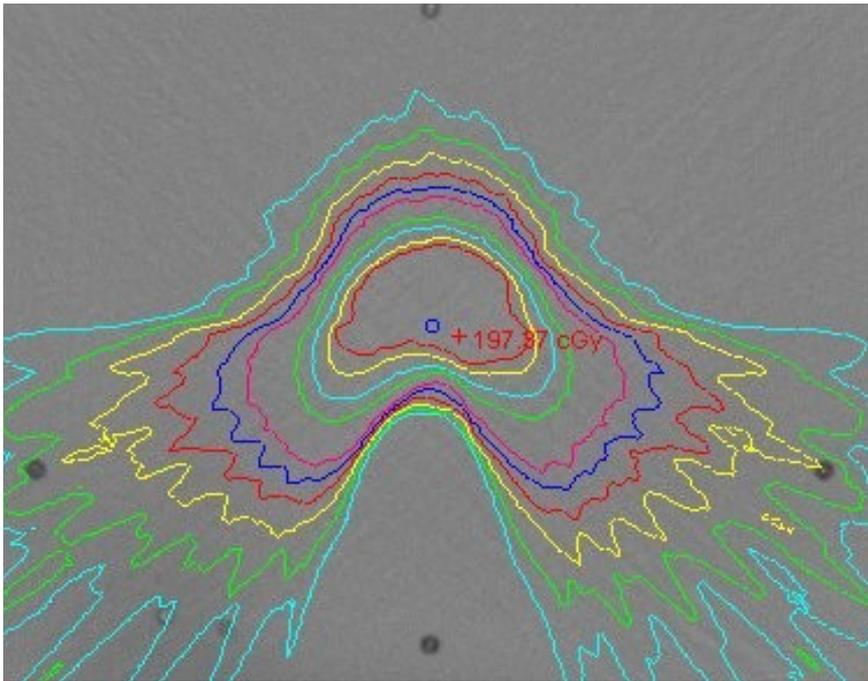


# Control de Calidad IMRT

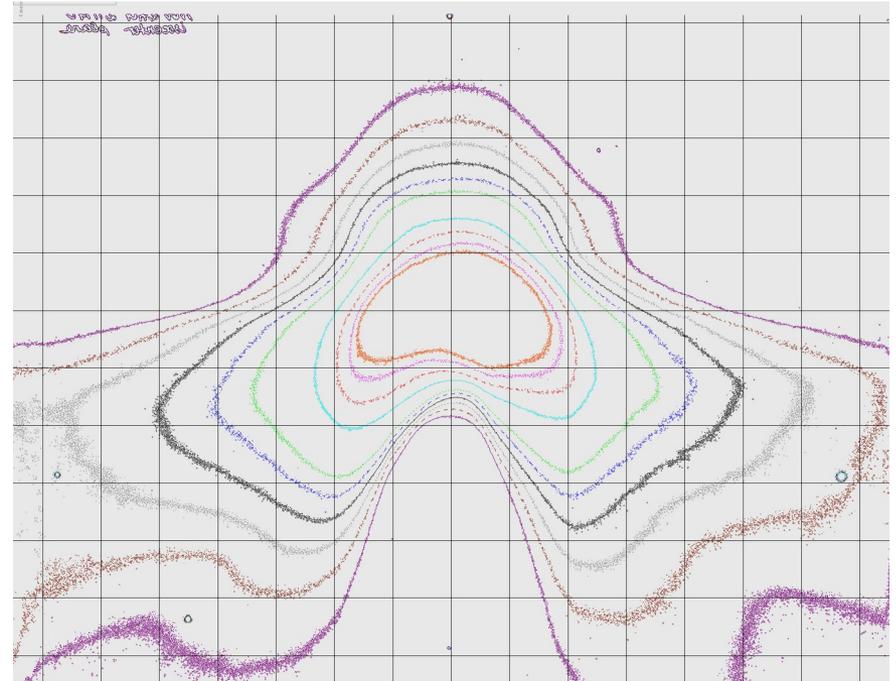
Paciente-Específico. Pruebas end-to-end



- Mediciones en un plano. Películas radiográficas  
Procesamiento (Comparación)



Calculada



Medida

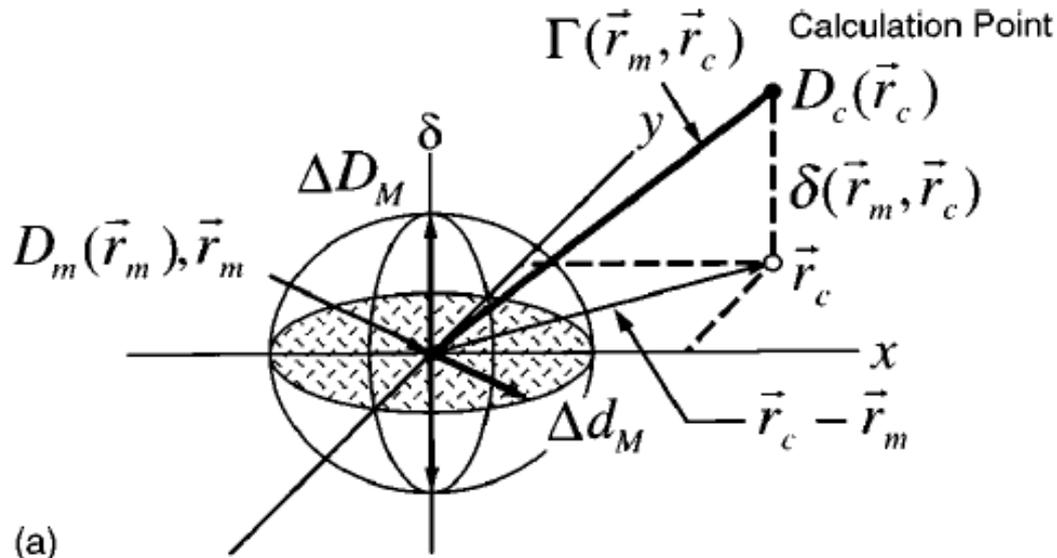
# Control de Calidad IMRT

Paciente-Específico. Pruebas end-to-end



- Mediciones en un plano. Películas radiográficas

Procesamiento (Métrica Gamma)



$$\Gamma(\mathbf{r}_m, \mathbf{r}_c) = \sqrt{\frac{r^2(\mathbf{r}_m, \mathbf{r}_c)}{\Delta d_M^2} + \frac{\delta^2(\mathbf{r}_m, \mathbf{r}_c)}{\Delta D_M^2}},$$

$$\gamma(\mathbf{r}_m) = \min\{\Gamma(\mathbf{r}_m, \mathbf{r}_c)\} \forall \{\mathbf{r}_c\},$$

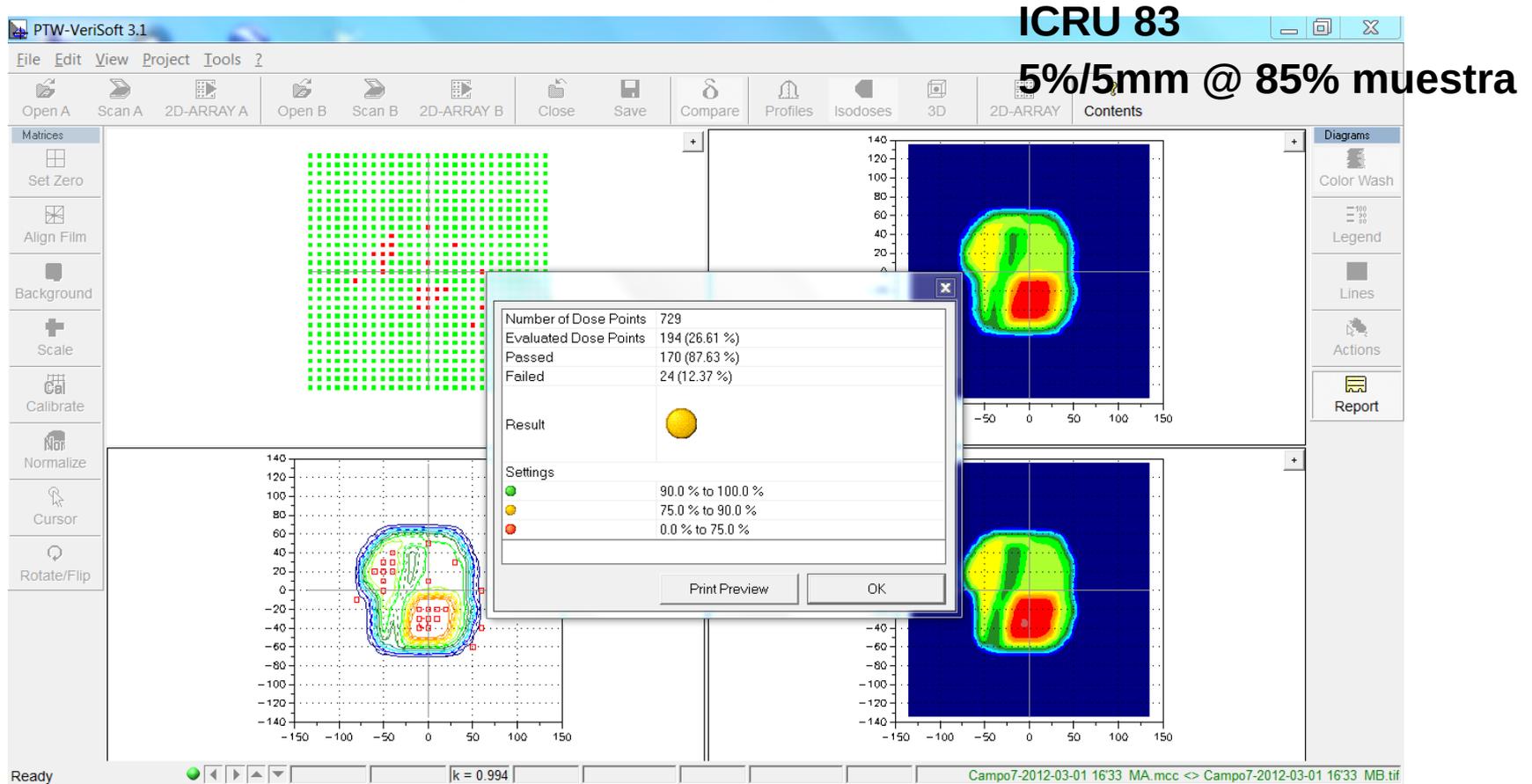


# Control de Calidad IMRT

## Paciente-Específico. Pruebas end-to-end



- Mediciones en un plano. Películas radiográficas  
Procesamiento (Comparación)



# Control de Calidad IMRT

## Paciente-Específico. Pruebas end-to-end



- Mediciones en un plano.

### Películas radiocrómicas vs radiográficas

#### Radiochromic Film

- Polymer-based
- Tissue equivalent
- Not sensitive to light
- Handle in room light
- Easy to position accurately
- Self developing
- Instant color change
  
- Store in dark envelope
- Watch temperature and humidity effect

#### Radiographic Film

- AgBr-based
- Not tissue equivalent
- Very sensitive to light
- Require dark room
- Difficult to position accurately
- Require processing
- Grey shades develop with processing
  
- Fixed after processing
- Not affected by temperature and humidity post processing

Radiochromic Film

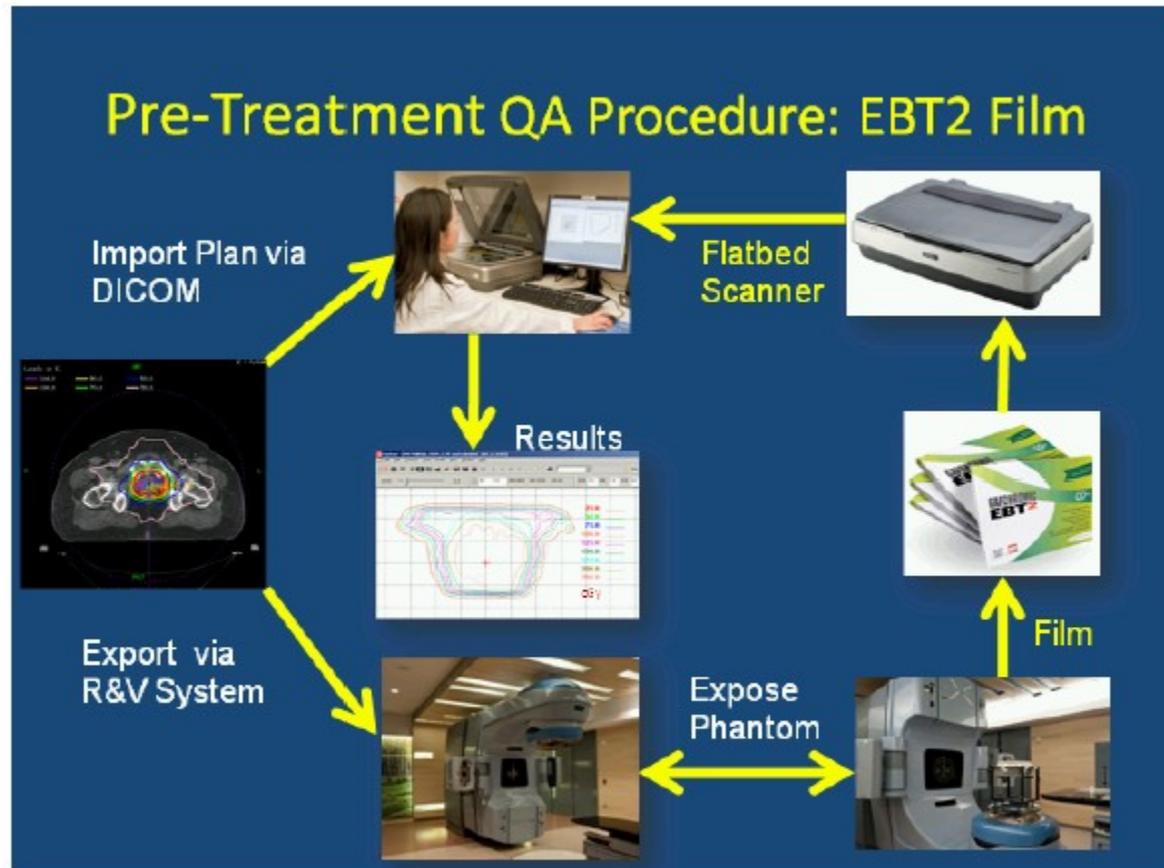
Radiographic Film

# Control de Calidad IMRT

## Paciente-Específico. Pruebas end-to-end

- Mediciones en un plano.

Películas radiocrómicas (procedimiento similar)



Pre-Treatment QA Procedure: EBT2 Film



# Computed Radiography Film

- **Active layer: photostimulable phosphor (BaSrFBr:Eu)**
- **Inserted in light tight envelope to avoid signal decay from room light exposure**
- **semi-logarithmic dose response up to 150cGy**
- **energy dependent leads to over-response of low energy scatter**

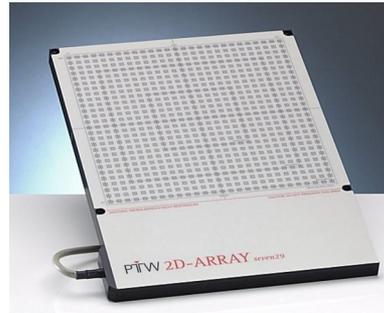
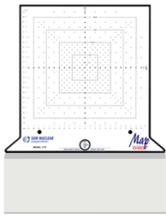


# Control de Calidad IMRT

Paciente-Específico. Pruebas end-to-end



- Mediciones en un plano. Arreglos bidimensionales de detectores



Sun Nuclear MapCHECK/3

PTW Seven29/ 1000 SRS  
/ 1500/ 1600 SRS

IBA Matrixx



Sun Nuclear  
StereoPhan+ SRS MapCHECK

IBA myQA SRS

# Control de Calidad IMRT

## Paciente-Específico. Pruebas end-to-end



- Mediciones en un plano. Arreglos bidimensionales de detectores.
  - Fluencia de dosis por campos

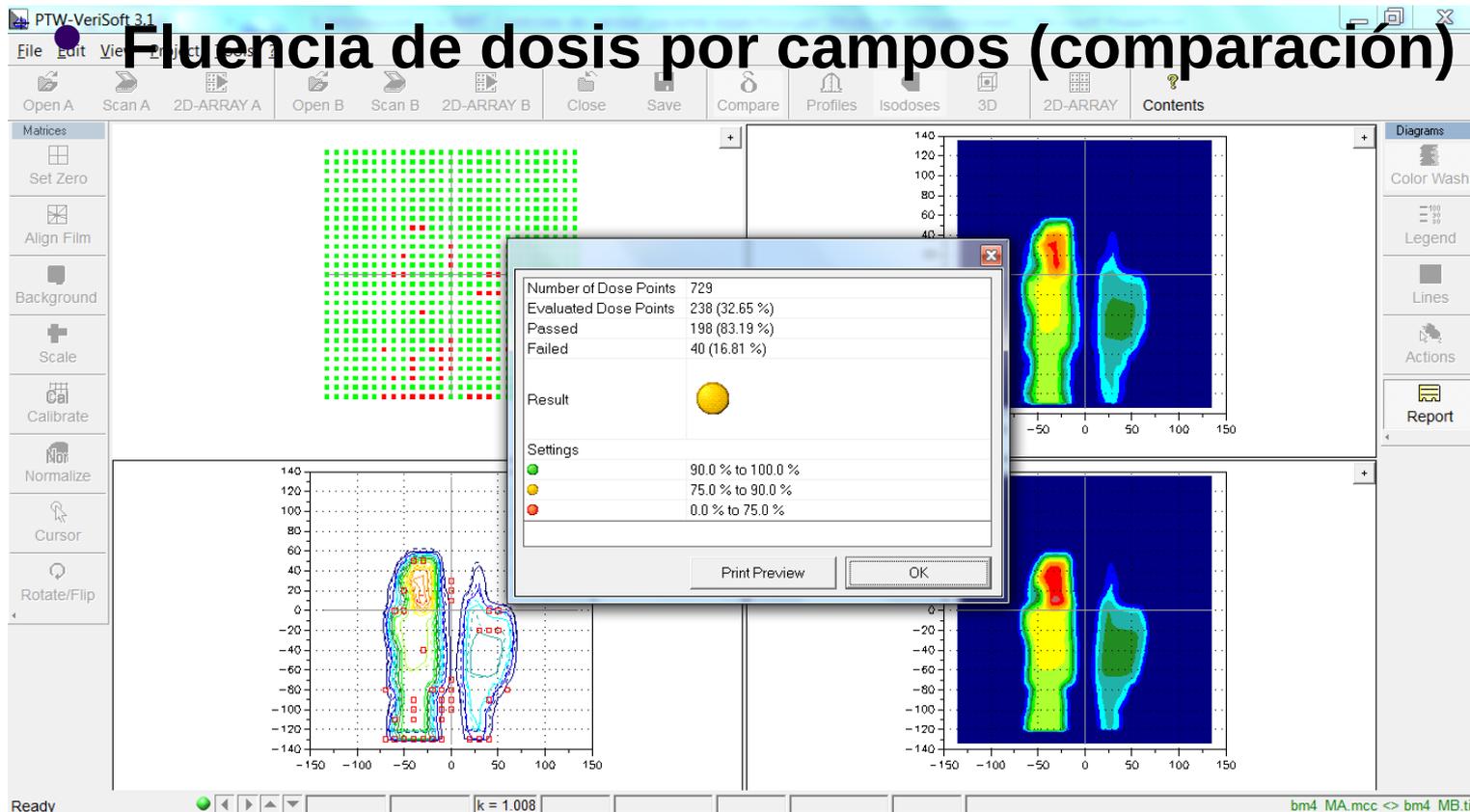


# Control de Calidad IMRT

## Paciente-Específico. Pruebas end-to-end



- Mediciones en un plano. Arreglos bidimensionales de detectores.



# Control de Calidad IMRT

## Paciente-Específico. Pruebas end-to-end



- Mediciones en un plano. Arreglos bidimensionales de detectores.
  - Fluencia de dosis compuesta (aporte de todos los campos de tratamientos). Precisa de correcciones por incidencia angular



### Address Rotational Beams

Use MapCHECK 3 with MapPHAN™, a water equivalent phantom, for RapidArc®, VMAT, and TomoTherapy®. Setup time is fast and measurement can occur in coronal and sagittal orientations.



### Outstanding Accuracy

- ✓ 50% more data points compared to previous MatrixXX detectors for highest IMRT & VMAT measurement resolution.
- ✓ Wireless Gantry Sensor+ enables precise QA of rotational cases and automated gantry angle correction.
- ✓ Confidence through independent QA.



# Control de Calidad IMRT

## Paciente-Específico. Pruebas end-to-end



- Mediciones compuestas
  - Fluencia de dosis compuesta (plan)



Sun Nuclear ArcCHECK



PTW OCTAVIUS 4D



IBA myQA SRS



ScandiDos DELTA4



Sun Nuclear  
StereoPhan+SRS MapCHECK

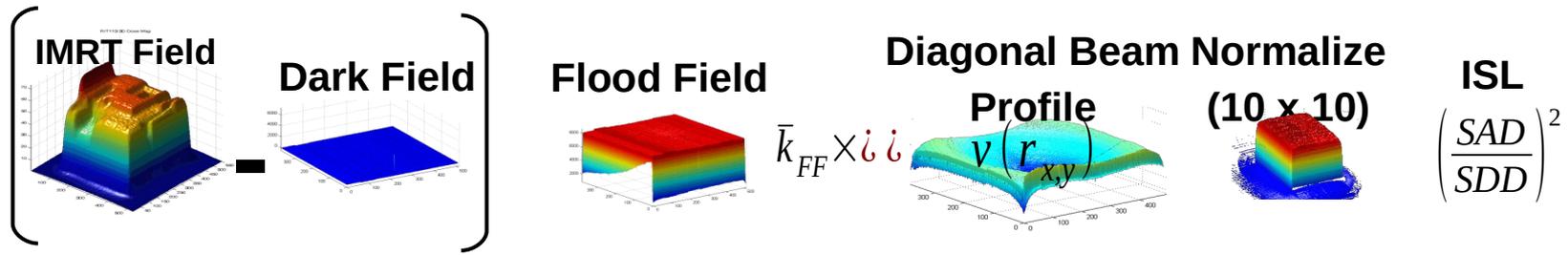
# Control de Calidad IMRT

## Paciente-Específico. Pruebas end-to-end



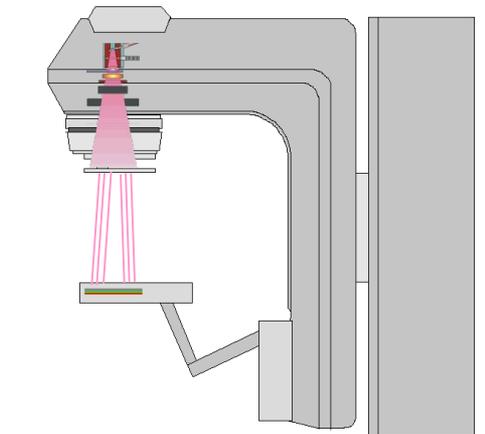
- Mediciones en un plano. Electronic Portal Image Device
  - Fluencia de dosis por campos (adquisición)

Raw EPID Image (IMRT field)



Comparison (in Matlab)  
and/or

Clinical Vision Review Environment



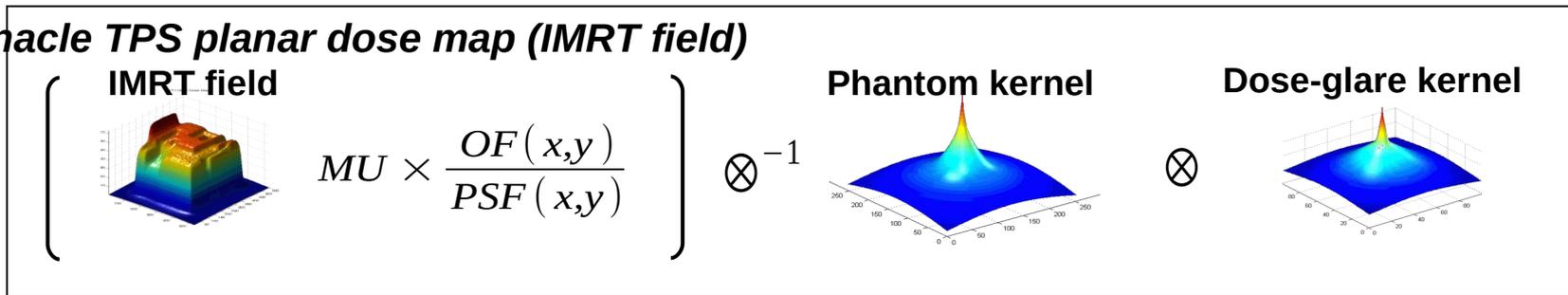
# Control de Calidad IMRT

Paciente-Específico. Pruebas end-to-end



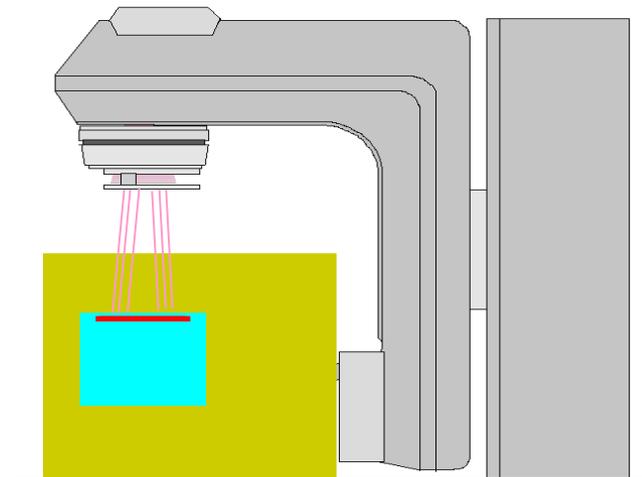
- Mediciones en un plano. Electronic Portal Image Device
  - Fluencia de dosis por campos (predicción del portal)

*Pinnacle TPS planar dose map (IMRT field)*



**Comparison (in Matlab)  
and/or**

**Clinical Vision Review Environment**

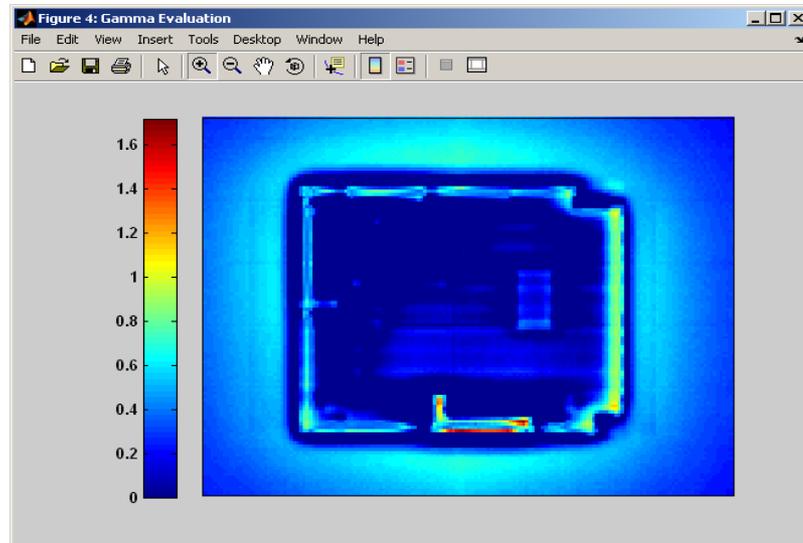
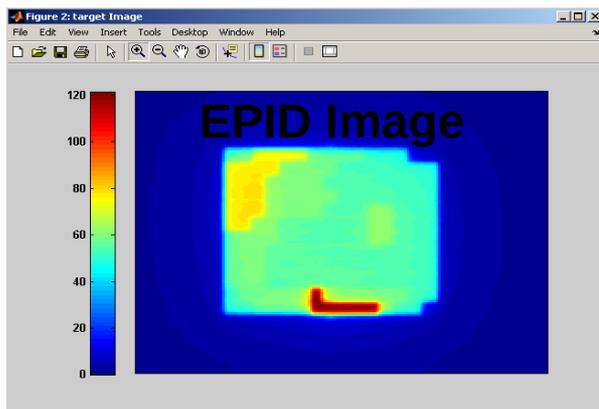
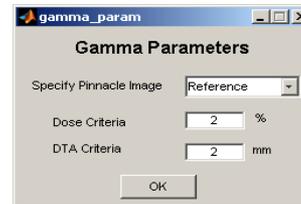
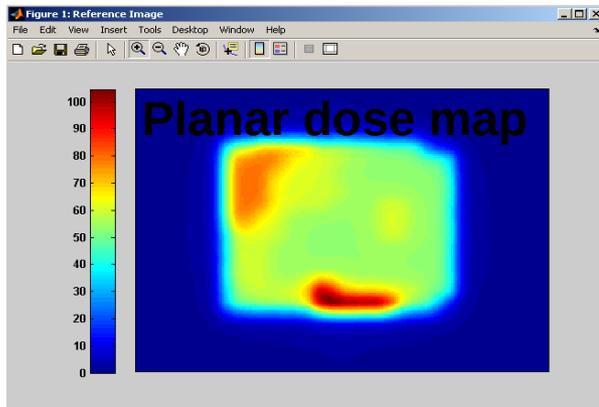


# Control de Calidad IMRT

## Paciente-Específico. Pruebas end-to-end



- Mediciones en un plano. Electronic Portal Image Device
  - Fluencia de dosis por campos (comparación)

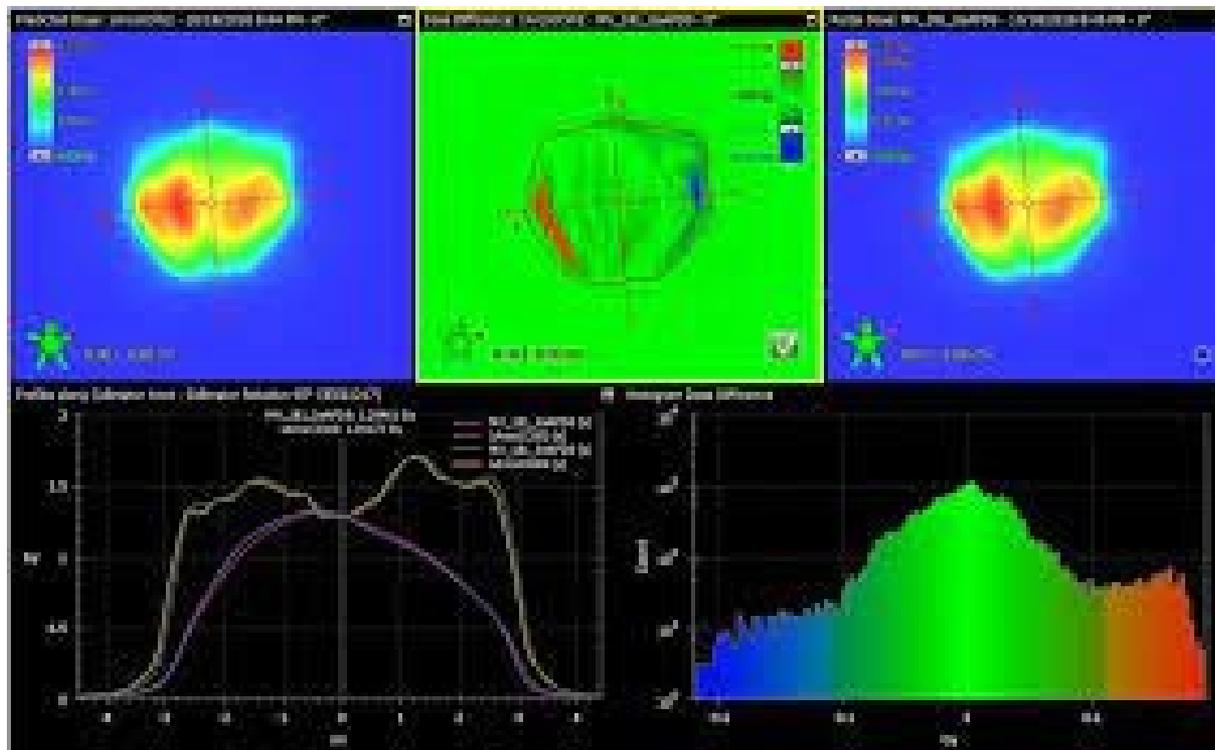


# Control de Calidad IMRT

## Paciente-Específico. Pruebas end-to-end



- Mediciones en un plano. Electronic Portal Image Device
  - Varian PortalDosimetry

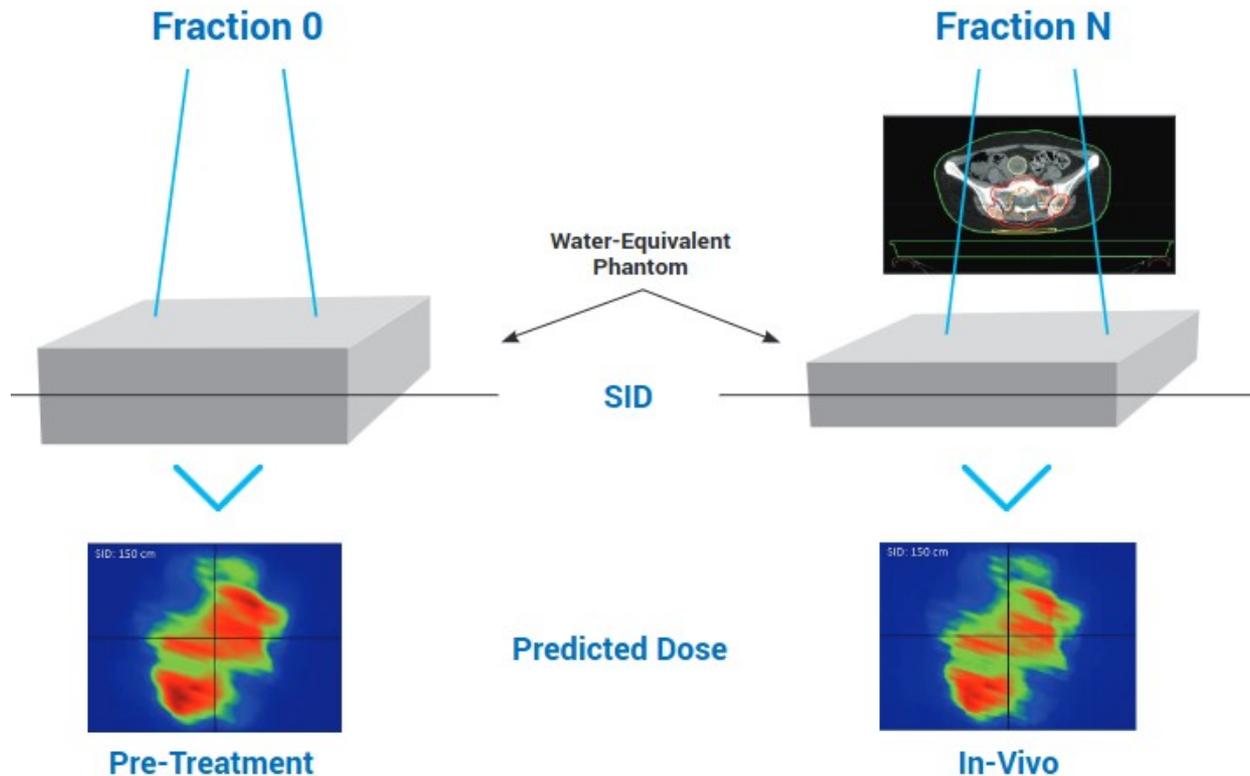


# Control de Calidad IMRT

Paciente-Específico. Pruebas end-to-end



- Mediciones en un plano. Electronic Portal Image Device
  - Sun Nuclear SUNCHECK, PerFRACTION

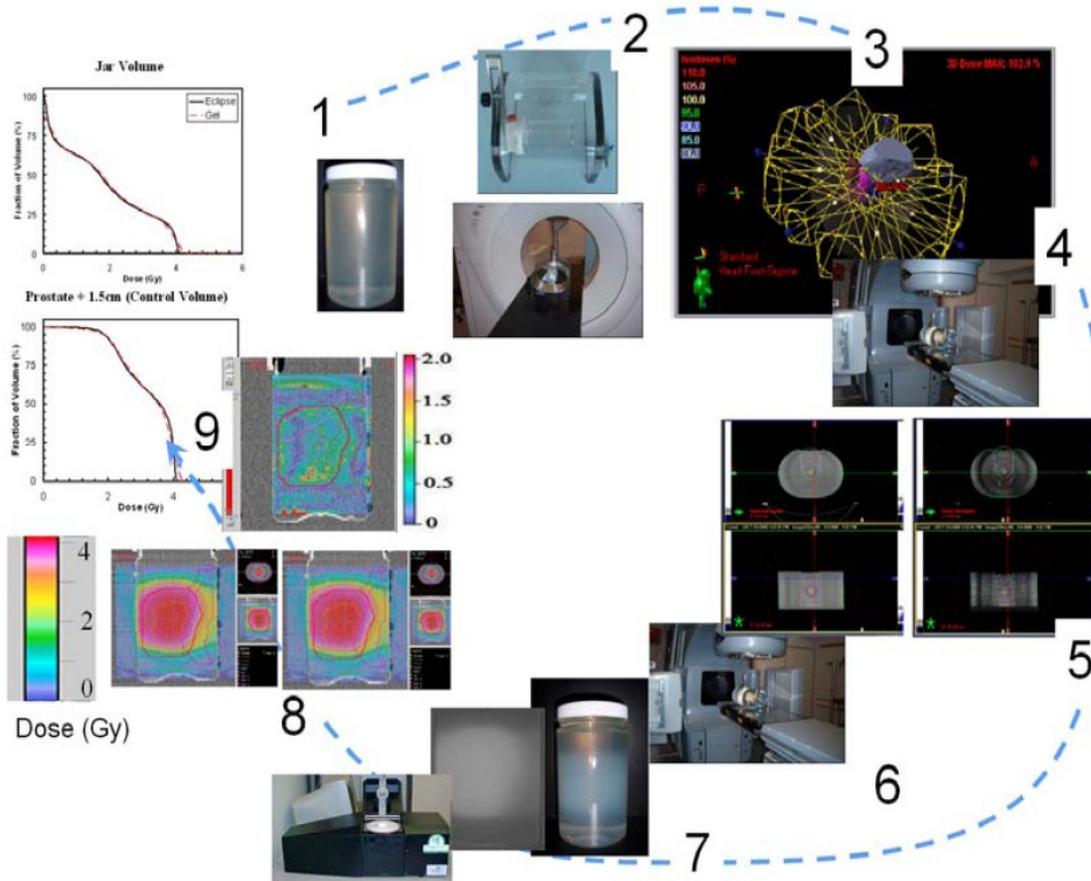


# Control de Calidad IMRT

## Paciente-Específico. Pruebas end-to-end



- Mediciones 3D. Gels





# 3D Dosimetry

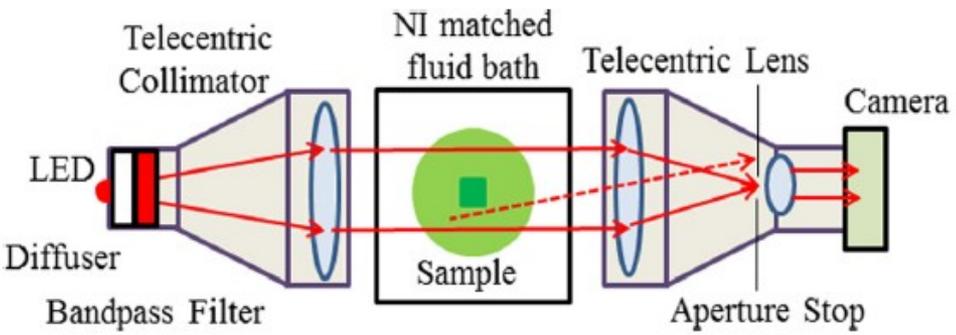
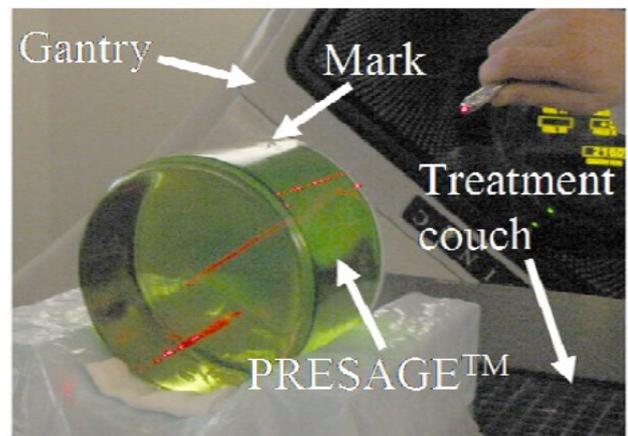


FIG. 1. Duke large field-of-view optical-CT scanner (DLOS). Light is collected by the matched telecentric imaging lens, which forms a precise image only from light rays that are parallel to the optic axis (with a  $0.1^\circ$  tolerance due to the aperture stop). Note rejected light rays due to the aperture such as the dashed scattered line. Each pixel in the image, measures the line-integral of optical attenuation through the dosimeter, with negligible scatter contamination upstream of the imaging lens.

**Figure 1.** PRESAGE™ dosimeter in treatment position (left image) and optical-CT scanner during imaging (right image). The arrow indicates the ray paths.

**New 3D dosimeters have overcome many of the challenges of prior 3D dosimeters: rigid, high resolution, no signal dispersion, no oxygen dependence**

**Dose can be read out quickly with new telecentric lens optical CT**



# Control de Calidad IMRT

## Paciente-Específico. ¿Futuro?



- **QA en su mayoría son pre-tratamiento**
  - Se asume el desempeño de la unidad es invariante
  - Se asume el paciente no cambia
- **Dosimetría in vivo**
- **IGRT**
- **Reconstrucción de dosis y DVH administrados**
- **Otras variantes (MLC trajectory log files)**

### Catching errors with *in vivo* EPID dosimetry

A. Mans,<sup>a)</sup> M. Wendling,<sup>b)</sup> L. N. McDermott,<sup>c)</sup> J.-J. Sonke, R. Tielenburg, R. Vijlbrief,  
B. Mijnheer, M. van Herk, and J. C. Stroom

*Department of Radiation Oncology, The Netherlands Cancer Institute—Antoni van Leeuwenhoek Hospital,  
Plesmanlaan 121, 1066 CX Amsterdam, The Netherlands*

# Control de Calidad IMRT

Paciente-Específico. Reconstrucción de dosis y DVH

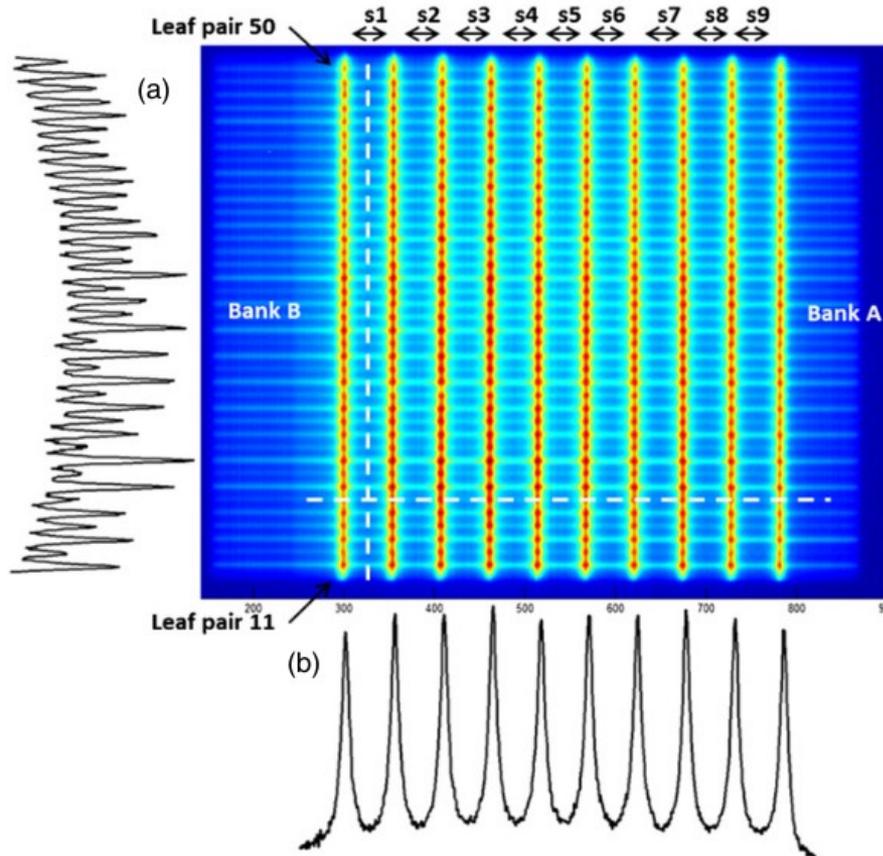


## Métodos

- **Algoritmo de reconstrucción directa**
  - IBA Compass, Sun Nuclear SunCHECK, PTW VERIQQA, PRIMO
- **Perturbación de la dosis planificada**
- **Reconstrucción en un maniquí**
  - OCTAVIUS 4D

# Control de Calidad IMRT

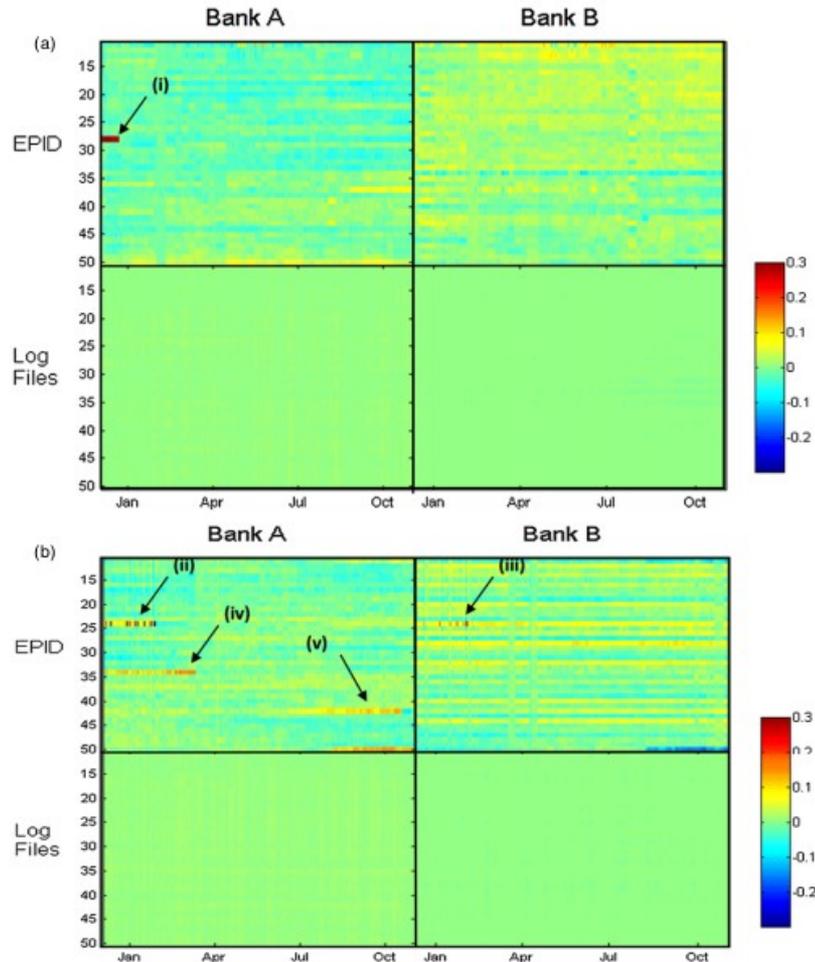
## Paciente-Específico. EPID y ficheros de registro



**Figure 1.** Picket fence test showing ten pickets (stripes), nine sub-sections (s1–s9), and profiles taken across (a) the leaves, and (b) the pickets.

# Control de Calidad IMRT

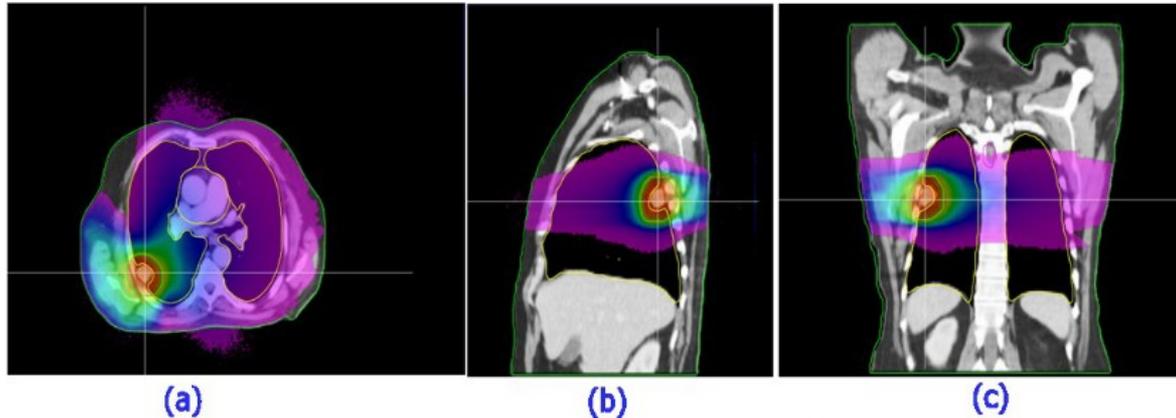
## Paciente-Específico. EPID y ficheros de registro



**Figure 5.** Leaf position errors over time for TB1 (a) and TB2 (b), analysed using both EPIDs and trajectory logs. X-axis represents time, Y-axis represents the leaf number, ranging from 10 to 50, and Z-axis (colour scale) represents the error in position.

# Control de Calidad IMRT

## Paciente-Específico. Ficheros de registro



**Figure 2.** The PRIMO simulated dose distribution for an SBRT plan in the axial (a), sagittal (b) and coronal (c) isocenter planes.

**Table 1.** Comparison of DVH parameters from PRIMO simulation and TPS. DVH – dose-volume histogram, PTV – planning target volume, SD- standard deviation, TPS- treatment planning system. MC- Monte Carlo.

DVH parameter	TPS(Acurus XB) Mean±SD	MC(PRIMO) Mean±SD	P-Value
PTV <sub>mean</sub> (Gy)	51.16 ± 0.85	51.31 ± 0.88	0.074
PTV <sub>max</sub> (Gy)	56.05 ± 2.11	57.37 ± 2.49	0.007
PTV D <sub>95</sub> (Gy)	46.74 ± 1.63	46.93 ± 1.61	0.169
LUNGS V <sub>20</sub> (%)	5.93 ± 1.42	5.79 ± 1.23	0.102
LUNGS V <sub>5</sub> (%)	19.31 ± 3.24	20.33 ± 3.39	0.061
LUNGS <sub>mean</sub> (Gy)	4.38 ± 0.68	4.38 ± 0.65	0.953
SPINE <sub>max</sub> (Gy)	12.00 ± 3.88	11.94 ± 3.95	0.541
CI	1.08 ± 0.04	1.09 ± 0.04	0.058
GI	4.31 ± 0.38	4.3 ± 0.40	0.683

**Table 2.** Comparison of DVH parameters from PRIMO dynalog reconstructed plan and TPS. DVH – dose-volume histogram, PTV – planning target volume, SD- standard deviation, TPS- treatment planning system. MC- Monte Carlo.

DVH parameter	TPS (Acurus XB) (Mean±SD)	MC(PRIMO) Mean±SD	P-Value
PTV <sub>mean</sub> (Gy)	51.16 ± 0.85	51.33 ± 0.92	0.093
PTV <sub>max</sub> (Gy)	56.05 ± 2.11	57.63 ± 2.89	0.009
PTV D <sub>95</sub> (Gy)	46.75 ± 1.65	47.05 ± 1.98	0.139
LUNGS V <sub>20</sub> (%)	5.93 ± 1.42	5.60 ± 1.34	0.083
LUNGS V <sub>5</sub> (%)	19.31 ± 3.24	20.63 ± 3.55	0.056
LUNGS <sub>mean</sub> (Gy)	4.38 ± 0.68	4.33 ± 0.67	0.484
SPINE <sub>max</sub> (Gy)	12.00 ± 3.88	12.17 ± 4.09	0.203
CI	1.08 ± 0.04	1.10 ± 0.04	0.101
GI	4.31 ± 0.38	4.45 ± 0.56	0.799

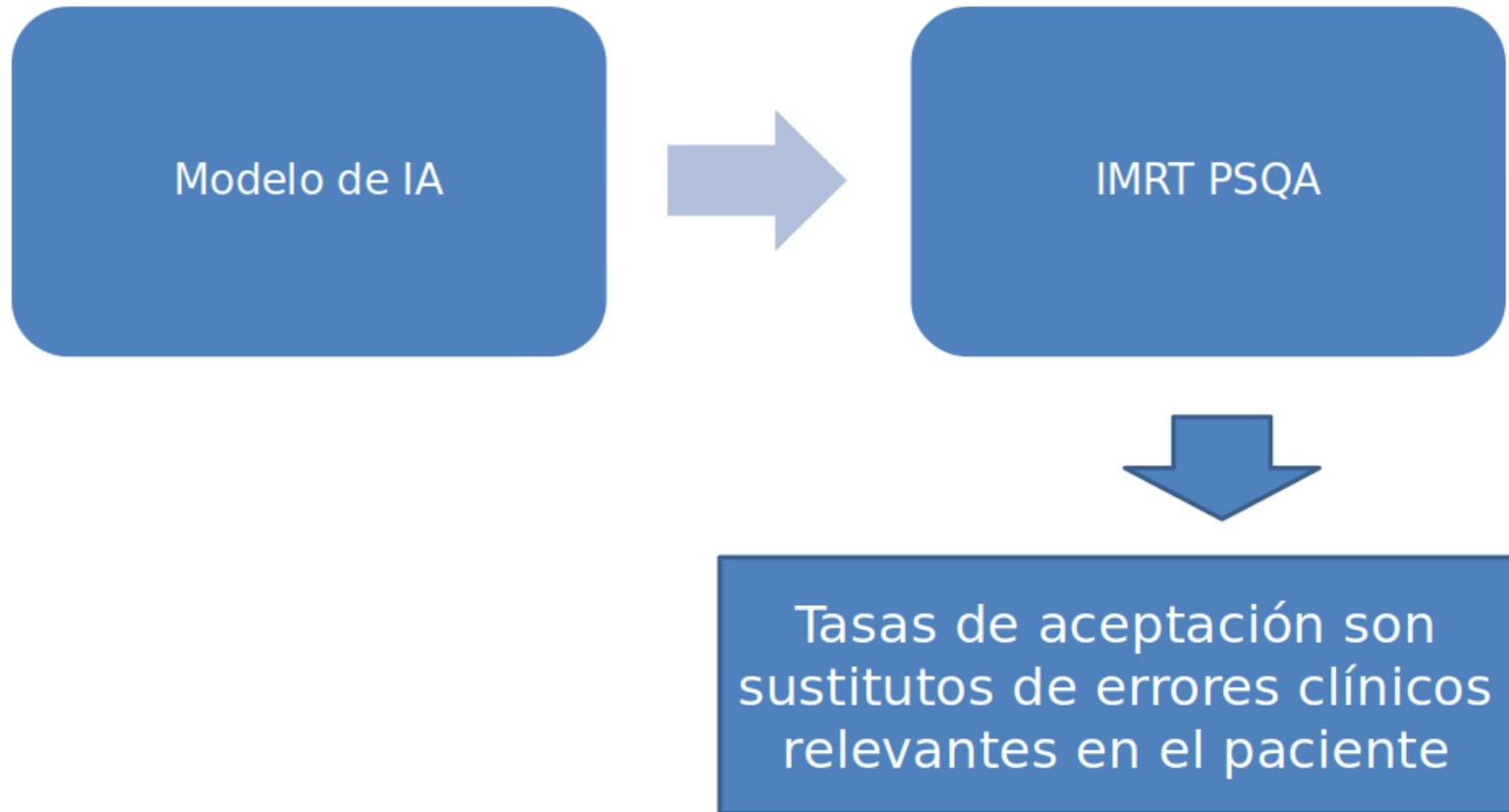
Clinical implementation of a PRIMO Monte Carlo-based dose verification and quality assurance model for stereotactic body radiotherapy (SBRT) treatment plans of the lung. Sarin B et al. Int. J. Radiat. Res. 2022

Treatment verification using Varian's dynalog files in the Monte Carlo system PRIMO. Rodriguez M, Brualla L. RO, 2019

# Control de Calidad IMRT

Paciente-Específico. Inteligencia Artificial

## ML IMRT PSQA



# Control de Calidad IMRT

Paciente-Específico. Inteligencia Artificial



## IMRT PSQA Paradigma

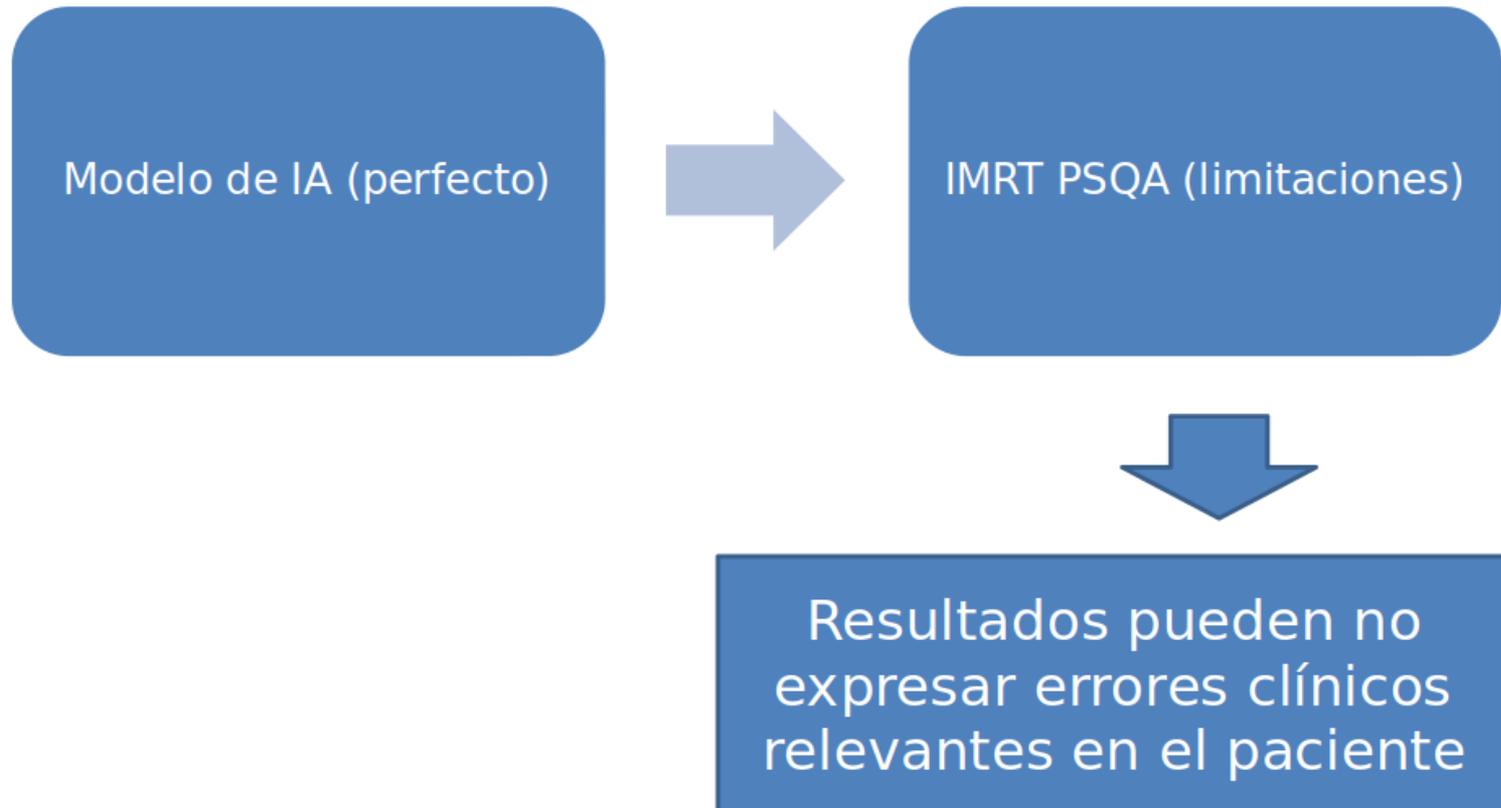
- **Múltiples fuentes de incertidumbres conjugadas en una medición única hacen retador desligar sus componentes individuales**
  - **Incertidumbres en el cálculo de dosis (modelado/limitaciones del algoritmo)**
  - **Desempeño de la unidad de tratamiento durante la administración**
  - **Calibración/Respuesta del detector**
  - **Configuración de medición**
    - **TC, PFF, PC**

# Control de Calidad IMRT

Paciente-Específico. Inteligencia Artificial



## ML IMRT PSQA Relevancia clínica



Evaluating IMRT and VMAT dose accuracy: Practical examples of failure to detect systematic errors when applying a commonly used metric and action levels. Nelms B. et al, Med Phys, 2013.



# Control de Calidad IMRT

Paciente-Específico. Inteligencia Artificial



## ML IMRT PSQA Ventajas

- **Reducir carga de trabajo a la unidad de tratamientos y el personal responsable**
- **La planeación de planes de IMRT puede ser más eficiente**
- **Aumentar la sensibilidad en la comprobación de los planes de IMRT**
- **Definir tasa de aceptación específicas por localizaciones anatómicas o estrategias de planeación**

# Control de Calidad IMRT

Paciente-Específico. Inteligencia Artificial



## ML IMRT PSQA Desventajas

- **Podemos confiar en los resultados del modelo de IA?**
  - **Depende de los datos de entrada utilizados**
  - **Modelo de IA**
- **Como detectar fallos en la predicción del modelo de IA?**
- **Como y por qué el modelo de IA predice el resultado en cuestión?**
  - **Interpretación**

# Control de Calidad IMRT

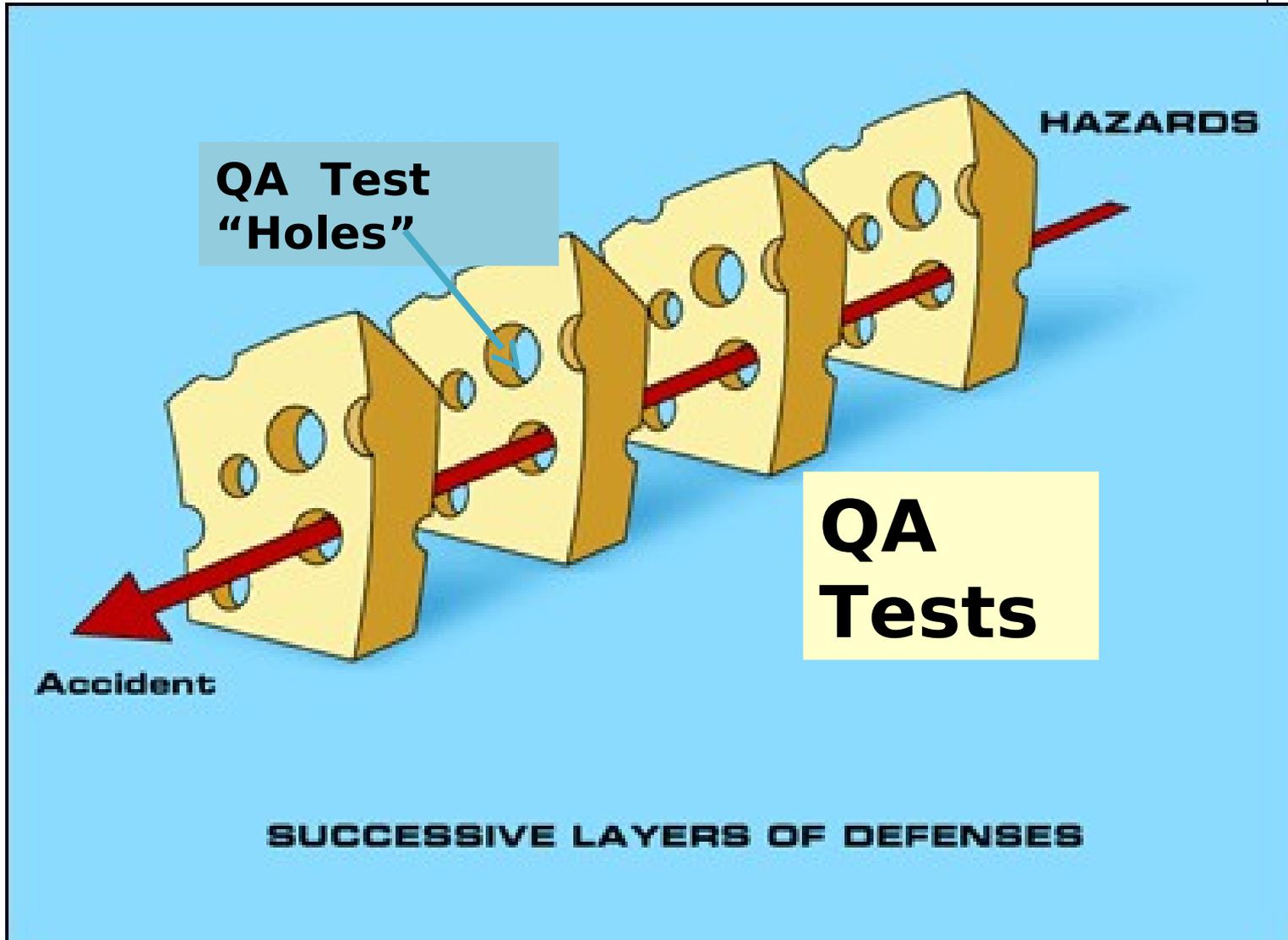
Paciente-Específico. Inteligencia Artificial



**ML IMRT PSQA Influencia en el flujo de trabajo**

- **Entrenar al modelo de IA puede suponer un considerable esfuerzo**
- **La planeación de planes de IMRT puede ser más complicada**
- **Aumento de la carga de trabajo en los procedimientos de QA a la unidad de tratamiento.**
- **Comprobación de otros parámetros ajenos al desempeño de la unidad de tratamiento, e.g. transmisión de datos en el sistema RV.**

# Accident Prevention



# Control de Calidad IMRT

## Paciente-Específico. Evaluación



- 7 casos reales
- Planeaciones IMRT/VMAT
- TG 119, 3 %/ 3 mm y Tasa de aceptación 88-90 %
- Resultados PSQA, Tasa de aceptación
  - Por campo, 99%
  - Plan compuesto, 93.4-100%
- Todos los casos presentaban errores sistemáticos
- Tipos de errores detectados
  - Configuración del modelo del algoritmo de cálculo
  - Limitaciones intrínsecas del algoritmo
  - Modelación y alineación del maniquí de QA en el TPS

# Control de Calidad IMRT

## Paciente-Específico. Evaluación



TABLE I. Details of the case studies, including TPS, linac, energy, MLC type, delivery modality, and type of error.

ID	TPS	Linac/MV/MLC	Delivery modality	Error type
1	Pinnacle	Elekta 6 MV 80-leaf (10 mm)	IMRT (step and shoot)	TPS model setting
2	MSK	Varian 6 MV 120-leaf	IMRT (dynamic)	TPS model setting
3	Eclipse	Varian 15 MV 120-leaf	IMRT (dynamic)	TPS input data
4A	Monaco	Elekta 6 MV 80-leaf (4 mm)	IMRT (step and shoot)	TPS algorithm
4B	Monaco	Elekta 6 MV 80-leaf (4 mm)	VMAT (1 arc)	TPS algorithm
5	Pinnacle	Varian 6 MV 120-leaf	VMAT (2 arc)	TPS algorithm
6	Pinnacle	Elekta 10 MV 80-leaf	Open field	TPS phantom setting
7	Eclipse	Varian 6 MV 120-leaf	VMAT (2 arc)	TPS phantom setting

**Evaluating IMRT and VMAT dose accuracy: Practical examples of failure to detect systematic errors when applying a commonly used metric and action levels. Nelms B. et al, Med Phys, 2013.**

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## Paciente-Específico. Evaluación



TABLE II. Passing rate method (per beam planar or composite), dosimeters, and analysis methods employed for each case study.

ID	Passing rate	Dosimeter(s)	Advanced diagnostic methods
1	Per-beam 2D	MapCHECK2	Dose profiles; 3D MGDR
2	Per-beam 2D	EPIDose	2%L/2 mm error pattern; 3D MGDR
3	Per-beam 2D	MapCHECK	2%L/2 mm error pattern; dose profiles; EPID-based
4A	Composite 3D	ArcCHECK	2%L/2 mm error pattern; dose profiles; 3D MGDR
4B	Composite 3D	ArcCHECK	2%L/2 mm error pattern; 3D MGDR
5	Composite 3D	Delta4; ArcCHECK	2%L/2 mm error patterns; dose profiles; 3D MGDR
6	Composite 3D	ArcCHECK	2%L/2 mm error pattern; ion chamber; 3D MGDR
7	Composite 3D	ArcCHECK	2%L/2 mm error pattern; 3D MGDR; dose grid inspection

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## Paciente-Específico. Evaluación



TABLE IV. Observed passing rates using the TG-119 instructions, i.e., 3%G/3 mm, 10% dose threshold, and (when available) measurement uncertainty turned “on.”

ID	Observed passing rates (%)	Details
1	99.2 ± 0.7 (1SD, range 98.1–99.8)	Mean over 7 IMRT beams
2	99.4 ± 1.2 (96.7–100)	Mean over 7 IMRT beams
3	99.3 ± 0.6 (98.9–100)	Mean over 5 IMRT beams
4A	96.6	Composite plan dose, 5 IMRT beams
4B	95.9	Composite plan dose, 1 VMAT beam
5	93.9 <sup>a</sup> , 94.7 <sup>b</sup>	Composite plan dose, 2 VMAT beams
6	97.8	Composite plan dose, 1 open field
7	100	Composite plan dose, 2 VMAT beams

<sup>a</sup>AC.

<sup>b</sup>Delta4.

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# Control de Calidad IMRT

## Paciente-Específico. Evaluación



### 3.B.1. Case Study 1: Incorrect TPS settings for leaf-end modeling

This case presented a 99.2% MapCHECK 3%/3 mm passing rate (averaged over all beams) for a head and neck

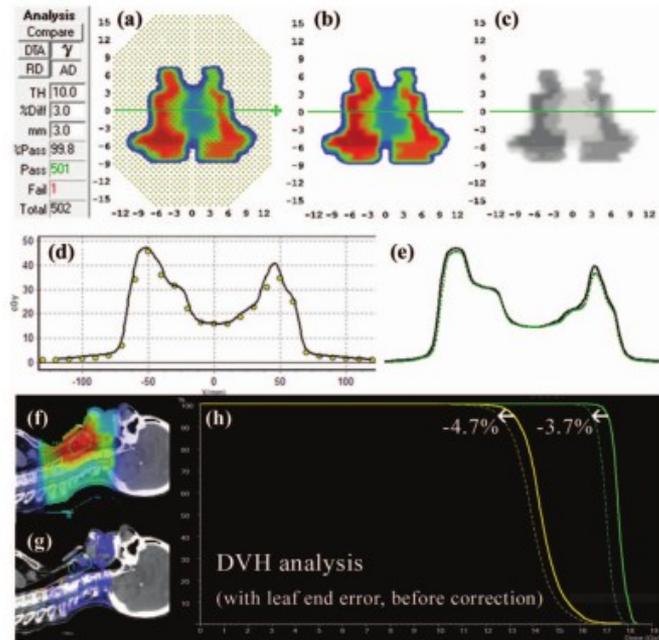


FIG. 1. Absolute dose planes at 10 cm depth, 100 cm source-detector-distance (SDD) shown for (a) measured and (b) calculated dose. (c) 3%/3 mm gamma failing points. (d) Dose profiles, dots represent calibrated diode measurements and solid lines the interpolated TPS profiles and (e) with measured profile (dotted) up-sampled using a commercial method (Refs. 12, 13, and 34). (f) Patient sagittal planar dose from TPS and (g) with 3DVH-estimated error showing lower estimated patient dose as dose difference, and (h) as shifts in DVH curves for two target volumes.

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# Control de Calidad IMRT

## Paciente-Específico. Evaluación



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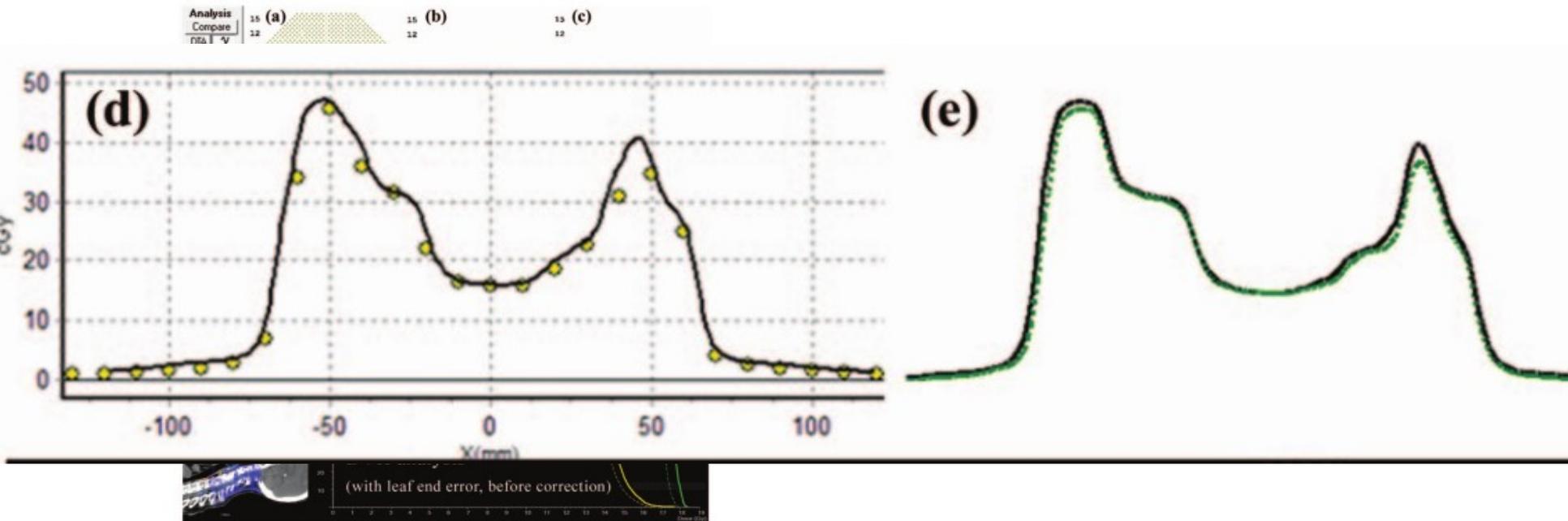


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# Control de Calidad IMRT

## Paciente-Específico. Evaluación



- Tasa de aceptación gamma 3 %/ 3 mm puede ser sub-óptima para la aceptación y puesta en servicio de técnicas de IMRT/VMAT
- Métricas más sensibles pueden identificar errores dosimétricos sistemáticos que de otra manera serían indetectables
- La adopción de métricas más sensibles y tolerancias más restrictas posibilitará:
  - el mejoramiento continuo de la exactitud en la administración de dosis en Radioterapia al nivel tanto del usuario final como del diseño del producto por el fabricante
  - la mejor estandarización de los métodos y procedimientos de aceptación y puesta en servicio del producto
  - Incrementar la calidad y reducir la variación, al punto de no ser necesarias las comprobaciones en masa

# Control de Calidad IMRT

## Paciente-Específico. Evaluación



### Tarea

- **Revisión bibliográfica del artículo referenciado**
- **Escoger dos de los casos restantes y hacer un informe explicando el error detectado, el método utilizado en la detección y las medidas tomadas para corregir el mismo (los casos no pueden solaparse en los informes individuales)**