

## Radiobiología. Aplicaciones en Radioterapia

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## Radiation Therapy Applications

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Slides courtesy of Jake Van Dyk, J. Battista and S. Karnas

## Main Goal of Radiation Therapy

# Maximize tumour control and minimize normal tissue effects

- Physics: dose distribution (gradients)
- Radiation biology: response of tissues to radiation Radiosensitizers/radioprotectors

## **Objectives/Outline**

- To describe the biological principles of radiation therapy
- To describe endpoints for measuring tumour and normal tissue response
- To be able to use mathematical models relating to tissue response
- To consider rationale for fractionated treatments
- To describe the effects of radiation-stimulated proliferation
- To describe the rationale for alternative fractionation

## **Clinical Example - Lung Cancer**



Radiation Therapy

- High dose to tumour/target
- Low dose to healthy tissues

## **Radiation Therapy**



## **Clinical Example - Brain Tumour**



## **Clinical Example - Prostate Cancer**



## **The Question**

- How do we optimize radiation treatment to maximize tumour control and minimize normal tissue effects?
- Need to understand and quantify:
  - Dose-response of tumour and normal tissue response
  - Factors influencing biological response
    - e.g., effects of dose, number of fractions, volume irradiated, ...

## **Response of Tissues to Radiation**

- Tumour response:
  - Regression
  - Cure or local control no regrowth
  - Regrowth/recurrence
- Normal tissue response:
  - Range of responses
    - Non-clinical e.g., observed on images
    - Mild symptoms discomfort
    - Life threatening or death

## **Tumour Size Nomogram**



Steel, 1997

## **Tumor Growth and factor affecting it**

Exponential growth: assuming constant growth rate

$$V = V_0 \ e^{\frac{\ln 2}{T_d} time}$$

- T<sub>d</sub> : tumour doubling time (Lung: 2-6 months, colorectal carcinoma: 2 y)
- GF: growth fraction (proliferating cells) (measured in tumor biopsies)
- $T_c$  : duration of cell cycle (~2 days for carcinoma)

Steel, 1997

- T<sub>pot</sub>: potential doubling time. Cell doubling time without any cell loss.
- $\Phi$ : cell loss factor,

 $\Phi = 1 - T_{pot}/T_d$ 

Table 3.1         Kinetic parame	ters of a typical human tumour
Cell cycle time ( $\approx 2$ d) Growth fraction ( $\approx 40\%$ )	$ \begin{cases} Potential \\ doubling \\ time (\approx 5d) \end{cases} Volume \\ doubling \\ doub$
Cell loss (≈90%)	time ( $\approx 70 \text{ d}$ )

## Tumor growth in a real world



Figure 2.3 Growth curves for tumours in rats and mice. The primary breast fibroadenomas and the Walker tumours were in rats, the others in mice. The fitted curves are Gompertz equations. From Steel (1977), with permission.

## More realistic models of tumor growth

### **Gompertzian growth:**

$$V = V_0 \exp\left[\frac{A}{B}(1 - e^{-Bt})\right]$$



Where  $V_0 =$  volume at time 0 A & B are parameters determining growth rate For small t, $V = V_0 \exp(At)$ Exponential GrowthFor large t, $V = V_0 \exp(A/B)$ Maximum Value

Logistic growth:

$$\frac{dV}{dt} = r.N \left(1 - \frac{V}{K}\right)$$

K: carrying capacity r: intrinsic rate of growth

## **Tumour Response to Radiation Treatment**



**Figure 2.8.** The volume response of an uncontrolled tumour is the resultant of two processes: regression and regrowth. Repopulation during the period of regression may take place at a rate that may differ from the growth rate of the untreated tumour.

Assays

Partial remission

Not preferred

Duration of disease free interval

- Preferred
- •Tumour growth delay (lab)
  - Preferred for measurable tumours

Steel, 1997

## **Tumor Control Probability (TCP)**

- Mechanistic models:
- TCP is usually described statistically by a Poisson distribution (Discussed by J. Battista in earlier lecture)

 $TCP = e^{-N_0 \times SF}$ 

- N<sub>0</sub>: initial number of cells.
- SF: surviving fraction. Depends on: dose, fractionation, cell sensitivity, repopulation,....

## **Tumor Control Probability (TCP)**

#### Empirical models:

Data analyses. No biological basis.Usually logistic regression is used.Typical example: TCP for NSCLC

 $TCP = rac{1}{1 + \left(rac{D50}{D}
ight)^{4\gamma}}$  (Martel et al., Lung Cancer, 24, 1999)

D<sub>50</sub>: dose to achieve 50% probability of control  $\gamma$  : normalized slop of the sigmoid curve at D<sub>50</sub>.



FIGURE 2. Recurrence-free survival percentage at 30 months. Lower (dashed) curve: as In Figure 1 Including repopulation with 2Gy given 5 fractions per week. Upper (full) curve: the same data after subtracting the effect of proliferation from the x-axis at 0.66 Gy/d from the 28th day after starting Irradiation of NSCLC, assuming Tk = 28 days, T<sub>p</sub> = 3 days, radiosensitivity ( $\alpha$  = 0.35 In/Gy and  $\alpha/\beta$  = 10 Gy. (Reprinted with permission from Elsevier Inc. Int J Radiat On-col Biol Phys<sup>35</sup>).

## **Normal Tissue Response**

### • Time of response:

Categories	Time	Caused by	Example	Repair
Early effects (tissues with rapid rate of turnover)	Few days or weeks	Death of large number of cells	Gastrointestinal epithelium, epidermal layer of the skin, hematopoietic system,	Rapid, usually reversible
Late effects	months or years	Damage to slowly proliferating tissues	Lung, kidney, heart, liver, CNS	Incomplete repair

## Normal Tissue Complication Probability (NTCP)

- Usually empirical with no mechanistic background
- Improving data sets is more problematic than deriving correct models.
- Lyman model: most widely used

$$NTCP(D,V) = \frac{1}{\sqrt{2\pi}} \cdot \int_{-\infty}^{u(D,V)} \exp\left(-\frac{1}{2}x^2\right) dx$$

 $TD_{50}(V) = \frac{TD_{50}(1)}{V^n}$  D

Dose producing 50% incidence

- $TD_{50}(1)$ : Uniform total dose to the whole which would lead to complication in 50 % of the population.
- $0 \le n \le 1$ : Volume effect (more pronounced for larger n values)
- m: inversely related to the steepness of the curve, 1998



## **Normal Tissue Complication Probability (NTCP)**



Joiner, 2009

## **Basic Principles of Radiation Therapy**

#### Favorable therapeutic ratio

#### Non Favorable therapeutic ratio



Ideal

Realistic

## **Therapeutic Ratio**



#### Therapeutic dose ratio = $D_2/D_1$

Want to maximize therapeutic ratio

- i.e., separate curves
- Parameters used to maximize the therapeutic ratio:
- Time, fractionation, hyperfractionation (greater sparing of late-responding normal tissue, radiosensitizers, cytotoxic agents, ),

## Therapeutic Index / Gain: with and without radiosensitizer



**Figure 1.4** The procedure by which an improvement in *therapeutic index* might be identified, as a result of adding chemotherapy to radiotherapy. *See also* Figures 12.3, 18.1.

Note: chemotherapy drugs can cause radiosensitivity

- 1. Decide the tolerance level (max permitted level of complication)
- 2. Find the optimal protocol that satisfies the tolerance level (B).
- 3. A proven therapeutic gain is achieved if B is statistically higher than A

#### Steel, 1997

## **Dose Fractionation**

- 4 R's radiobiology
  - Repair of sublethal damage
  - Reassortment
  - Repopulation
  - Reoxygenetion
- Dividing dose in no. fractions <u>spares</u> normal tissues
  - Repair normal tissue
  - Repopulation of normal tissue
- Dividing dose in no. fractions *increases* damage to tumour
  - Reoxygenation
  - Reassortment into radiosensitive phases

## Late responding tissues are more sensitive to fractionation



Figure 9.1 Relationship between total dose and dose per fraction for a variety of normal tissues in experimental animals. The results on late-responding tissues (full lines) are systematically steeper than those on early-responding tissues (broken lines). Chart from Hall (1988) quoting the data of Thames *et al* (1982), with permission.



## **Recall LQ Model For Cell Survival**



 $S = e^{-(\alpha D + \beta D^2)}$ 

Where D = dose  $\alpha$ ,  $\beta$  are parameters defining curvature  $\alpha$  defines initial slope  $\alpha/\beta$  [Gy]

## Late versus Early reacting tissues in terms of the LQ Model



 Late responding tissues show higher fractionation sensitivity.

P. Mayles, 2007

## Fractionation: early vs late responding tissues



Figure 8.3 Schematic survival curves for target cells in (a) acutely responding and (b) late-responding normal tissues. The abscissa is radiation dose on an arbitrary scale. From Thames and Hendry (1987), with permission. Joiner, 2009

- Effect E: reduction in cell survival that is equivalent to tissue tolerance.
- Because the survival curve for late responding tissues is more curvy, the isoeffective total dose increases more rapidly with increasing number of fractions.
- **BED** is the dose that produces E for an infinite # of very small doses

## Fractionation

- The difference in steepness of isoeffect curves between early and late responding tissues can be described by a single parameter: α/β.
- Late responding tissues are more sensitive to changes in fraction size. α/β is small.
- Early responding tissues (including tumour) are less sensitive to changes in fraction size. α/β is large.
- Some tissues are more sensitive than others for any chosen dose per fraction. α and β varies with tissue type.

α/µ (Fron	ratios from lab data n Thames and Hend	a ry)
Early Reactions	<b>High</b> α/β: ~10*	α/β
skin hair follicles lip mucosa jejunum colon testis spleen *prostate exceptio	on	9.4 - 21.0 5.5 - 7.7 7.9 7.1 8.4 13.9 8.9 3.0
Late Reactions	Low α/β: mostly ~3	
spinal cord brain eye kidney bladder lung bowel		2.1 - 5.2 2.1 1.2 0.4 - 4.1 7.2 - 7.8 2.1 - 4.3 3.0 - 5.0

#### Table 9.1 Fractionation sensitivity of human normal tissues and tumours

Tissue/organ	Endpoint	α/β (Gy)	95% CL (Gy)	Source
arly reactions				
Skin	Erythema	8.8	6.9; 11.6	Turesson and Thames (1989)
	Erythema	12.3	1.8; 22.8	Bentzen et al. (1988)
	Dry desguamation	~8	N/A	Choqule and Supe (1993)
	Desquamation	11.2	8.5; 17.6	Turesson and Thames (1989)
al mucosa	Mucositis	9.3	5.8; 17.9	Denham et al. (1995)
	Mucositis	15	- 15; 45	Rezvani et al. (1991)
	Mucositis	~8	N/A	Chogule and Supe (1993)
te reactions				
n/vasculature	Telangiectasia	2.8	1.7; 3.8	Turesson and Thames (1989)
	Telangiectasia	2.6	2.2; 3.3	Bentzen <i>et al.</i> (1990)
	Telangiectasia	2.8	-0.1; 8.1	Bentzen and Overgaard (1991)
ocutis	Fibrosis	1.7	0.6; 2.6	Bentzen and Overgaard (1991)
ast	Cosmetic change in appearance	3.4	2.3; 4.5	START Trialists Group (2008)
	Induration (fibrosis)	3.1	1.8; 4.4	Yarnold et al. (2005)
iscle/vasculature/ artilage	lmpaired shoulder movement	3.5	0.7; 6.2	Bentzen <i>et al.</i> (1989)
rve	Brachial plexopathy	<3.5*	N/A	Olsen <i>et al.</i> (1990)
	Brachial plexopathy	~2	N/A	Powell et al. (1990)
	Optic neuropathy	1.6	-7; 10	Jiang e <i>t al.</i> (1994)
nal cord	Myelopathy	<3.3	N/A	Dische <i>et al.</i> (1981)
2	Corneal injury	2.9	-4; 10	Jiang e <i>t al.</i> (1994)
wel	Stricture/perforation	3.9	2.5; 5.3	Deore <i>et al.</i> (1993)
wel	Various late effects	4.3	2.2; 9.6	Dische <i>et al.</i> (1999)
g	Pneumonitis	4.0	2.2; 5.8	Bentzen <i>et al.</i> (2000)
	Lung fibrosis	3.1	-0.2; 8.5	Dubray et al. (1995)
	(radiological)			
ad and neck	Various late effects	3.5	1.1; 5.9	Rezvani e <i>t al.</i> (1991)
ad and neck	Various late effects	4.0	3.3; 5.0	Stuschke and Thames (1999)
oraglottic larynx	Various late effects	3.8	0.8; 14	Maciejewski et al. (1986)
cavity + oropharynx	Various late effects	0.8	-0.6; 2.5	Maciejewski e <i>t al.</i> (1990)
nours				
a and neck		10.5	6 5: 20	Sturshke and Thomas (1000)
anous		14.5*	0.5; 29	Remoni et al. (1992)
arynx oeal oord		~12	4.3, 24 'wide'	Robertson et al (1002)
luccal mucosa		~13	2.9:00	Macielewski et al. (1993)
onsil		7.2	2.9,00	Maciejewski et al. (1989)
lasonhan/ny		16	- 11: 42	lee et al (1995)
in in		85*	4.5.11.2	Trott et al (1984)
ostate <del>l</del>		1.1	-3.3.5.6	Bentzen and Bitter (2005)
reast		46	11.81	START Trialists Group (2009)
sophagus		4.9	1.5:17	Geh et al. (2006)
elanoma		0.6	-1.1:2.5	Bentzen <i>et al.</i> (1989)
inosarcoma		0.4	-14:54	Thames and Suit (1996)
ciposarcoma		0.4	-1.4, 5.4	manies and built (1960)

CL, confidence limit.

\*Re-analysis of original published data.

Fseveral more estimates are available from comparisons of outcome after brachytherapy versus external-beam therapy. Reference details are available from Søren Bentzen. See also Thames et al. (1990) and Table 13.2.



The alfa and beta of tumours: a review of parameters of the linear-quadratic model, derived from clinical radiotherapy studies. van Leeuwen et al. Radiation Oncology (2018) 13:96

## The LQ isoeffect equation

What change in total radiation dose is required when we change the dose per fraction?

Isoeffective fractionations:

$$E = (\alpha . d_1 + \beta . d_1^2) . n_1 = (\alpha . d_2 + \beta . d_2^2) . n_2 \longrightarrow \frac{D_1}{D_2} = \frac{d_1 + \frac{\alpha}{\beta}}{d_2 + \frac{\alpha}{\beta}}$$

• Equivalent dose in 2 Gy fractions (EQD<sub>2</sub>):

$$EQD_2 = D \frac{d + \frac{\alpha}{\beta}}{2 + \frac{\alpha}{\beta}}$$

The dose in 2Gy fraction that is biologically equivalent to a total dose D given with a fraction size of d.  $\boldsymbol{\alpha}$ 

EQD<sub>2</sub> allows comparing the effectiveness of different treatment regimens with total doses and doses per fraction. It is used to normalize TCP and NTCP as well as DVHs.

## **Iso-Effect Curves**



## **Biologically Effective Dose (BED)**

$$S = e^{-(\alpha D + \beta D^2)}$$

$$S = e^{-n(\alpha d + \beta d^2)}$$

Effect, E = -ln(S)

 $E = \alpha d + \beta d^{2} \text{ for 1 fraction}$  $E = nd(\alpha + \beta d) \text{ for } n \text{ fractions}$ 

$$BED = \frac{E}{\alpha} = nd(1 + \frac{d}{\alpha / \beta}) \quad [Gy_{\alpha/\beta}]$$

BED is not a real dose

As  $d \rightarrow 0$ ,  $n \rightarrow \infty$ , Then BED =  $n \times d = D$  on x-axis

BED is the total dose which if given in infinitely small fractions is equivalent to the actual fractionated regimen with dose per fraction d and total dose D.

- BED is regarded as a measure of the true biological dose delivered by particular combination of dose per fraction and total dose to a given tissue characterized by a specific α/β ratio.
- Even if D is kept constant, the BED will increase if d increases.
- The BED for each tissue (α/β ratio) is a measure of the extent to which the dose can be escalated if treating with very small d.

## **Biologically Effective Dose (BED)**

Assume a standard dose fractionation: 30 fraction X 2 Gy = 60Gy. what is the permitted dose per fraction in case n = 20?

$$BED = 100 Gy_3 = 20d(1 + \frac{d}{3})$$
 d = 2.65 Gy; D = 53 Gy

What is the effect of a hot spot of 110% in the normal tissue? The resultant BED=138.6 Gy<sub>3</sub>

Biological doses are enhanced proportionally more than the physical doses at hot spots due to the quadratic term in the LQM ("double trouble" effect).

For large volumes with inhomogeneous dose distributions, BED calculations should not be based on one single reference point.

## **BED** Explained Further

- BED allows "normalization" of bio-effects to a common reference quantity (infinite number of small doses).
- BED's for different exposures can be added biologically
- Useful quantity when radiation treatments are interrupted or intentionally split
- See the additional explanations and illustrations in DropBox Folder "Reference \_Material"

So far, we have ignored Repair and Repopulation..

### Ejemplo 1

¿Cuál será el número de fracciones que es necesario impartir en un esquema de tratamiento dado a 3 Gy por fracción, 1 fracción al día, 5 días a la semana para que sea equivalente a un tratamiento en el que se imparten 50 Gy a 2 Gy por fracción, 1 fracción al día, 5 días a la semana? Consideraremos un valor de  $\alpha/\beta = 10$  Gy para efectos de respuesta precoz y tejidos tumorales y un valor de  $\alpha/\beta = 3$  Gy para efectos de respuesta tardía de los tejidos sanos.



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## Ejemplo 2

En un tratamiento se administran 54 Gy en 16 fracciones, 1 fracción al día, 5 días a la semana. ¿Cuál será la dosis equivalente administrada en 2 Gy por fracción, 1 fracción al día, 5 días a la semana con respecto a los efectos tardíos de los tejidos sanos?



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## Ejemplo 3

Sobre un tumor de cabeza y cuello se planifica un tratamiento de 60 Gy en 30 fracciones a 2 Gy por fracción, una fracción al día, 5 días a la semana. En este tratamiento original la médula recibe 48 Gy y la piel 60 Gy durante el tratamiento. Por un error dosimétrico, durante las 10 primeras fracciones del tratamiento tanto el tumor, como la médula y la piel reciben 2,5 Gy por fracción. Una vez detectado el error se decide continuar el tratamiento conforme a la planificación inicial. ¿Cuántas fracciones de 2 Gy según la planificación original habrá que administrar para conseguir un tratamiento equivalente al previsto? Consideraremos la fibrosis subcutánea como efecto tardío en la piel  $(\alpha/\beta = 2 \text{ Gy})$ , la mielopatía de la médula espinal  $(\alpha/\beta = 3 \text{ Gy})$  y un valor de  $\alpha/\beta = 10$  Gy para el tumor. No se tendrá en cuenta el efecto de la proliferación.

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